Neural targets for relieving parkinsonian rigidity and bradykinesia with pallidal deep brain stimulation

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Clinical evidence has suggested that subtle changes in deep brain stimulation (DBS) can have differential effects on bradykinesia and rigidity in patients with Parkinson’s disease. In this study, we first investigated the degree of improvement in bradykinesia and rigidity during targeted globus pallidus DBS in three 1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine (MPTP)-treated rhesus macaques. Behavioral outcomes of DBS were then coupled with detailed, subject-specific computational models of neurons in the globus pallidus internus (GPI), globus pallidus externus (GPe), and internal capsule (IC) to determine which neuronal pathways when modulated with high-frequency electrical stimulation best correlate with improvement in motor symptoms. The modeling results support the hypothesis that multiple neuronal pathways can underlie the therapeutic effect of DBS on parkinsonian bradykinesia and rigidity. Across all three subjects, improvements in rigidity correlated most strongly with spread of neuronal activation into IC, driving a small percentage of fibers within this tract (<10% on average). The most robust effect on bradykinesia resulted from stimulating a combination of sensorimotor axonal projections within the GP, specifically at the site of the medial medullary lamina. Thus the beneficial effects of pallidal DBS for parkinsonian symptoms may occur from multiple targets within and near the target nucleus.

Parkinson’s disease; globus pallidus
behaviorally across a range of stimulation voltages and electrode configurations. Computational neuron models of DBS (Johnson and McIntyre 2008) were tailored to each subject’s brain anatomy and were used to investigate how modulation of the pallidofugal and IC pathways influences behavioral outcome measures of parkinsonian limb rigidity and bradykinesia.

MATERIALS AND METHODS

Animals. We studied three female rhesus macaques (Macaca mulatta). All surgical procedures and behavioral protocols were approved by the Institutional Animal Care and Use Committee of the Cleveland Clinic and complied with United States Public Health Service policy on the humane care and use of laboratory animals.

Surgical procedures. Using aseptic surgical procedures under isoflurane anesthesia, mild to moderate hemiparkinsonian states were induced through unilateral intracarotid infusions of MPTP (0.4–0.6 mg/kg over a 10-min period). In two of the three nonhuman primates (NE and RA), additional intramuscular injections of MPTP were administered to augment parkinsonian motor symptoms (0.2–0.4 mg/kg daily treatment over a 4- to 5-day period). All three animals reached a moderately parkinsonian state (Fig. 1A) such that akinesic symptoms did not prevent them from performing a reach-and-retrieval task for food reward.

Neurosurgical planning incorporated computed tomography (CT) scans and T1/T2-weighted magnetic resonance images acquired from each animal under propofol anesthesia (Micocinovic et al. 2007). Surgical procedures used to implant the cranial chambers and implantable pulse generators (IPG) are described in detail elsewhere (Hashimoto et al. 2003; Johnson et al. 2009). The smaller 17-mm DBS chamber held a 30–35° angle from vertical in the coronal plane. An IPG (Medtronic Itrel II) was placed subcutaneously below the scapula, and an extension cable was routed subcutaneously between the IPG and the DBS chamber. Analgesics were provided before and after these procedures.

Following a recovery period, microelectrode recordings were performed through the DBS chamber to verify coordinates and boundaries of each pallidal segment before DBS lead implantation. Microdrive-guided insertions were made with a single tungsten microelectrode (FHC) or a linear array of 12 microelectrodes on a tungsten drive-guided insert. Tissue track for each pallidal segment before DBS lead implantation. Microelectrode configurations. Computational neuron models of DBS behaviorally across a range of stimulation voltages and electrode configurations. Computational neuron models of DBS (Johnson and McIntyre 2008) were tailored to each subject’s brain anatomy and were used to investigate how modulation of the pallidofugal and IC pathways influences behavioral outcome measures of parkinsonian limb rigidity and bradykinesia.

**Fig. 1. Characterization of parkinsonian motor signs in the deep brain stimulation-implanted (DBS-OFF) state.** A: the average severities of parkinsonian motor signs were evaluated before 1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine (MPTP) treatment and again following MPTP treatment and DBS lead implantation (3: severe; 0: no symptoms). The number of testing sessions is given by n in each case. Scores are reported as ±SE following MPTP treatment in the DBS-OFF state. MPTP treatment elicited a moderate parkinsonian state in each subject. Bradykinesia (B) and finger dexterity (C) were quantified in terms of performance on a reach-and-retrieval task for food reward. Following administration of MPTP, movements became significantly slower, and the ability to manipulate small objects became impaired. Uni, unilateral; Sys, systemic.

Before and after implantation of the DBS lead, baseline parkinsonian motor scores were collected using a modified version of the Unified Parkinson’s Disease Rating Scale (UPDRS) to ensure that a substantial therapeutic effect did not occur from the implantation process (Fig. 1A). An examiner, who was blinded to the condition of the animal, rated the severity of the animals’ rigidity, akinesia, resting tremor, posture, and gait (0, no symptoms, to 3, severe symptoms). Scores were averaged over multiple behavioral testing sessions, each consisting of observing the animal sitting in a chair and ambulating in a plastic enclosure. Akinesia was assessed by the amount of spontaneous movement over a 30-min interval. Although each of these parkinsonian symptoms was present at varying degrees in the three animals, we only evaluated rigidity and bradykinesia (slowness of movement) in the context of DBS.

Rigidity and bradykinesia were evaluated in baseline sessions and during DBS sessions. With the nonhuman primate awake and resting comfortably in its chair, an examiner blinded to the applied DBS setting assessed muscle rigidity according to the degree of resistance to passive movements of the elbow, shoulder, hip, and knee joints contralateral to the implanted DBS lead (0, no symptoms, to 3, severe symptoms). Rigidity scores were averaged across joints for each session. Bradykinesia was assessed through a self-paced, reach-and-

<table>
<thead>
<tr>
<th>Subject</th>
<th>NE</th>
<th>MA</th>
<th>RA</th>
</tr>
</thead>
<tbody>
<tr>
<td>Profile</td>
<td>♂, 5.0 kg</td>
<td>♂, 5.5 kg</td>
<td>♂, 4.9 kg</td>
</tr>
<tr>
<td>Age</td>
<td>10 yrs</td>
<td>8 yrs</td>
<td>9 yrs</td>
</tr>
<tr>
<td>Treatment</td>
<td>Uni/Sys</td>
<td>Uni/Sys</td>
<td>Uni/Sys</td>
</tr>
<tr>
<td>R rigidity</td>
<td>2.1 ± 0.2 (n=15)</td>
<td>1.0 ± 0.2 (n=17)</td>
<td>1.5 ± 0.2 (n=10)</td>
</tr>
<tr>
<td>Akinesia</td>
<td>1.8 ± 0.5 (n=10)</td>
<td>1.1 ± 0.4 (n=16)</td>
<td>1.9 ± 0.3 (n=32)</td>
</tr>
<tr>
<td>Tremor</td>
<td>0.9 ± 0.3 (n=14)</td>
<td>2.1 ± 0.4 (n=16)</td>
<td>1.1 ± 0.5 (n=32)</td>
</tr>
<tr>
<td>Posture</td>
<td>2.0 ± 0.3 (n=12)</td>
<td>1.4 ± 0.2 (n=10)</td>
<td>2.0 ± 0.0 (n=20)</td>
</tr>
<tr>
<td>Gait</td>
<td>1.5 ± 0.3 (n=11)</td>
<td>1.6 ± 0.2 (n=10)</td>
<td>1.5 ± 0.2 (n=20)</td>
</tr>
</tbody>
</table>

Total (15) | 8.3 | 7.2 | 8.0 |
retrieval task for food reward. Video of each trial was recorded at 30 frames per second, and frame-by-frame analysis was used to calculate and differentiate the movement time of each trial, defined as the summation of reach and retrieval times, from manipulation time (Johnson et al. 2009). Comparisons between a pre-MPTP state and a post-MPTP/DBS-implanted (DBS-OFF) state showed significant increases in movement time and time to grasp the food reward (Fig. 1, A and C), which is consistent with bradykinesia and impaired fine manipulation in human PD (Berardelli et al. 2001). These two measures (rigidity and bradykinesia) were used for all DBS-OFF/ON trials.

DBS-ON sessions were conducted at least 1 mo after lead implantation to reduce susceptibility of the voltage fields to known changes in electrode-tissue impedances (Lempka et al. 2009). Stimulation settings consisted of a sustained pulse train at 135 Hz with charge-balanced pulses (90-μs long cathodic phase, 3.5-ms long anodic phase). Voltages ranged from 0 to 3 V for monopolar and 0 to 6 V for bipolar configurations. Multiple trials were conducted over multiple days for each DBS setting. Parkinsonian motor signs were examined after 1–5 min of stimulation. In the case when multiple DBS settings were examined on a single testing session, trials were separated by at least 10 min of no stimulation. Several factors constrained the number of DBS settings that could be examined during the programming process, including the necessity for washout periods following DBS and the induction of contralateral muscle contractions during DBS at higher voltages. A summed total of 87 different simulation parameter sets were investigated.

**Neuron and electrical field models.** A nonhuman primate brain atlas (Martin and Bowden 2000) was edge-warped to preoperative MR images (Edgewarp). Surface reconstructions of the external and internal GP were generated in a three-dimensional nonuniform rational basis spline modeling environment (Rhinoceros). The MRI-based reconstructions were adjusted with minor scale and translation corrections to match the borders of the nuclei identified during microelectrode mapping sessions. Stimulation sites were mapped onto the MRI images (Edgewarp). The borders of the identified pallidal segments were estimated within the specific territories of each subject's GPe and GPi were estimated within the posterolateral portion of each pallidal segment according to 1) each subject's sensorimotor responses observed during microelectrode mapping sessions and 2) sensorimotor regions identified through previous histological studies (Francois et al. 1994; Hoover and Strick 1993). Computational neuron models of GPe and GPi were developed in the context of each subject's sensorimotor region. Analysis of the computational model parameter space was constrained to those sensorimotor regions of GP. Model parameters and properties for the pallidal neurons were consistent with those reported previously (Johnson and McIntyre 2008). In addition to the pallidal neuron models, axonal models of motor-related IC fibers (mIC; n = 100) were developed in the context of each subject's MRI-based reconstruction of IC and were distributed uniformly and posterior to the capsule genu (Schmahmann and Pandya 2006). The IC myelinated axon models were represented with nodes of Ranvier (NODE), myelin attachment segments (MYSA), paranode main segments (FLUT), and internode segments (STIN). As previously described (McIntyre et al. 2002), the nodes were instantiated with a membrane capacitance as well as nonlinear fast Na⁺, persistent Na⁺, slow K⁺, and linear leak conductances. Both MYSA and STIN

The computational neuron models, described in detail elsewhere (Johnson and McIntyre 2008), consisted of a population of GPe and GPi neurons that were reconstructed from nonhuman primate biotinylated dextran amine-labeled pallidal neurons (Parent et al. 2001; Sato et al. 2000; Fig. 2). These morphologies were converted into a series of compartments with lengths and thicknesses defined individually for the soma, dendrites, and axons of the pallidal neurons. The GPe neuron morphologies were distributed randomly within the reconstruction of each subject's GPe such that the axonal processes passed either through GPi (n = 370) or directly into the IC (n = 630) as mentioned in the figure. The GPi neurons (n = 1,000) were randomly distributed within the nucleus such that their axonal processes coursed medially along the lenticular fasciculus or ansa lenticularis (Baron et al. 2001; Parent and Parent 2004). The sensorimotor territories of each subject's GPe and GPi were estimated within the posterolateral portion of each pallidal segment according to 1) each subject's sensorimotor responses observed during microelectrode mapping sessions and 2) sensorimotor regions identified through previous histological studies (Francois et al. 1994; Hoover and Strick 1993). Computational neuron models of GPe and GPi were distributed within their respective pallidal segments and labeled according to whether their soma was located within a sensorimotor region. Analysis of the computational model parameter space was constrained to those sensorimotor regions of GP. Model parameters and properties for the pallidal neurons were consistent with those reported previously (Johnson and McIntyre 2008). In addition to the pallidal neuron models, axonal models of motor-related IC fibers (mIC; n = 100) were developed in the context of each subject's MRI-based reconstruction of IC and were distributed uniformly and posterior to the capsule genu (Schmahmann and Pandya 2006). The IC myelinated axon models were represented with nodes of Ranvier (NODE), myelin attachment segments (MYSA), paranode main segments (FLUT), and internode segments (STIN). As previously described (McIntyre et al. 2002), the nodes were instantiated with a membrane capacitance as well as nonlinear fast Na⁺, persistent Na⁺, slow K⁺, and linear leak conductances. Both MYSA and STIN

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**Fig. 2.** A computational model of globus pallidus (GP)-DBS (Johnson and McIntyre 2008). The model provided a quantitative prediction of the local cellular effects of DBS in the GP and internal capsule (IC). A: coronal view of the overall model system, which consists of populations of GP externus (GPe), GP internus (GPi), and motor-related IC (mIC) neurons. Shown are single reconstructions of each neuron type. GPe neurons projected either to subthalamic nucleus (STN) directly through IC or through GPi before projecting through IC. B–D: the neuron models consisted of multiple compartments instantiated with passive and active membrane properties in the soma, dendrites, and axon segments. See Johnson and McIntyre (2008) and McIntyre et al. (2002) for more details on the neuron models. Note that the fiber diameters are not drawn to scale. NA⁺, fast Na⁺; h, hyperpolarization-activated cyclic nucleotide-gated (HCN) channel; Cm, membrane capacitance; gmy, myelin sheath conductance; cmy, myelin sheath capacitance; gNa, Na⁺ channel; gK, K⁺ channel; gKC, cyclic nucleotide-gated (HCN) channel; gKCa, Ca²⁺-activated K⁺ channel; IC, internal capsule; STIN, internode segments; FLUT, paranode main segments; MYSA, myelin attachment segments; NODE, nodes of Ranvier.
segments were modeled with a parallel circuit containing a membrane capacitance and linear conductance. The FLUT segments consisted of similar passive membrane properties with the addition of a fast $K^+$ conductance.

A model of the implanted DBS lead was positioned within the pallidal reconstruction according to a coregistration of preoperative MRI and postoperative CT imaging. Neurons with model compartments found to overlap spatially with the DBS lead were removed from subsequent analysis. An axisymmetric finite-element model simulating the voltage distribution of DBS in neural tissue was applied in COMSOL Multiphysics (Johnson and McIntyre 2008; Miocinovic et al. 2006). The model consisted of a 57% voltage drop at the electrode-tissue interface and a 250-μm thick encapsulation layer (0.18 S/m) between the electrode and bulk tissue (0.20 S/m; Miocinovic et al. 2009). In the NEURON v6.1 programming environment (Hines and Carnevale 1997), multicompartment cable models of sensorimotor GPe and GPi neurons and mIC fibers were simulated with the amplitude of the filtered extracellular stimulation waveform scaled by the finite-element model voltage distributions (Johnson and McIntyre 2008).

**Statistical analysis.** Statistical analyses (ANOVA, $P < 0.05$) were performed for comparisons between clinically rated parkinsonian motor symptom scores in the normal and post-MPTP/DBS-OFF states. These tests were also used to investigate differences in each subject’s motor performance on a reach-and-retrieval task. In the three subjects investigated in this study, on average, increasing the voltage of DBS resulted in a decrease in the severity of parkinsonian motor signs up until the voltage-induced contralateral muscle contractions, which confounded the therapeutic effect. The relationships between model predictions and behavioral outcome measures were thus estimated to be second-order in nature. These relationships were examined with polynomial regression analysis and with $F$-test statistics to investigate whether the second-order regression explained a significant proportion of the variance ($P < 0.05$).

**Histology.** At the conclusion of the experiments, the animals were deeply anesthetized, given an overdose of pentobarbital (100 mg/kg), and perfused with a 10% paraformaldehyde solution. The brains were removed and processed with histological techniques (50-μm sections in either coronal or sagittal planes and Nissl-stained). For each animal, the DBS lead location was identified within the histological slices, which in all three cases validated the imaging-based results of the DBS lead within the GP (Fig. 3).

**Fig. 3.** DBS lead localization in the GP. A–C: volumetric reconstructions of the leads within the GP were generated by coregistration and segmentation of preoperative MRI and postoperative computed tomography scans (inset). Histology (inset) was also performed for each lead implant. Stereotactic implantation coordinates for the DBS leads were established by means of microelectrode recordings in which regions of putamen, GPe, GPi, and optic tract were each identified. Cube markers represent cells identified as responsive to sensorimotor manipulation. D: sensorimotor regions (cross-hatched regions) of GPe and GPi and optic tract were each identified. 3D: sensorimotor territories of GPe and GPi were estimated from these recordings as well as from previous histological studies (Francois et al. 1994; Hoover and Strick 1993). D, dorsal; M, medial.
RESULTS

Estimation of the DBS parameter space. The anatomic coordinates and orientations of the three DBS leads were implanted along different trajectories through the GP, which enabled stimulating a diverse population of GPe and GPi neurons across the three subjects (Fig. 3, A–C). The DBS lead in subject NE had its three proximal electrode contacts in GPi and its distal electrode contact near the border of optic tract. The DBS lead in subjects MA and RA had its two middle electrode contacts in GPe primarily. For both of these implants, the distal electrode contact was located slightly medial to the medial medullary lamina, with the proximal contact at the border between GPe and putamen. To target a larger proportion of GPe efferents projecting directly into IC en route to STN, the DBS lead in subject RA was positioned near the medial border of GPe and IC. In contrast, the DBS lead in subject MA was positioned more ventral and posterior to sample a larger proportion of GPe efferents projecting through GPi.

Segmentation of the GPe and GPi was further demarcated into sensorimotor and nonsensorimotor territories as described in MATERIALS AND METHODS (cross-hatched and non-cross-hatched portions, respectively, in Fig. 3D). The volumetric reconstruction of the DBS lead was positioned within this framework according to each subject's histology and postoperative CT scan. All three DBS leads were found to overlap spatially with a small percentage of the total number of GPe and GPi model neurons (GPe, GPi; NE: 6.4, 7.1%; MA: 5.9, 2.1%; RA: 5.0, 1.1%) and a slightly larger percentage of GPe and GPi model neurons within the sensorimotor territory in each pallidal segment (NE: 17.0, 12.0%; MA: 11.1, 4.6%; RA: 9.3, 3.7%).

Computational neuron models of mIC fibers were also simulated for all DBS settings evaluated in the nonhuman primates, including those settings that were at or above threshold for inducing contralateral muscle contractions in the upper and lower limbs. The models predicted that 10.8 ± 3.5% of mIC fibers were activated on observing contralateral muscle contractions, a percentage that was consistent across animals and across electrode configurations (Fig. 4A). To assess the degree to which DBS in each monkey was able to activate one pathway over another, the modeling results underwent correlation analysis. Overall, the models predicted that a broad combination of pallidal neuron to IC fiber activation could be evaluated behaviorally in the nonhuman primates (Fig. 4B). Specifically, across the three subjects, there was a positive correlation between activation of GPe output and activation of GPi output for all DBS settings due in large part to activation of GPe neurons projecting through GPi (Fig. 4, C–F). Subjects MA and RA also showed positive correlations between activation of GPe and mIC as well as activation between GPi and mIC pathways. However, in the case of subject NE, there was no clear relationship between activation of mIC fibers and either GPe or GPi pathways suggesting that stimulation settings could dissociate activation of those pathways.

Identification of therapeutic pallidal DBS settings. The severity of parkinsonian rigidity and bradykinesia was quantified for a range of DBS settings, which consisted of variations in both electrode configuration and stimulation amplitude. Pulse width and frequency were unchanged. A total of 87 different
stimulation settings were examined behaviorally across the 3 subjects (42 for rigidity and 55 for bradykinesia with 10 settings common between the 2 behavioral examinations). Thresholds for evoking muscle contractions with stimulation were observed between −2 and −3 V for cathodic-monopolar DBS and −4 and −7 V for bipolar DBS. Muscle contractions first appeared as either an orofacial (RA) or upper extremity (NE and MA) contraction, likely reflecting slightly different anterior-to-posterior implant trajectories (Landy et al. 2000).

Although improvement in rigidity and bradykinesia with pallidal DBS was observed in all three subjects, the degree of improvement depended on the precise electrode configuration and applied stimulation voltage (Fig. 5). Increasing the DBS voltage resulted in a progressive improvement in rigidity for all electrode configurations even at small voltages in subject NE and RA. For all other cases (rigidity in subject MA and bradykinesia in all 3 subjects), symptoms remained unchanged at low stimulation voltages and improved at higher voltages. We observed that further increase in stimulus amplitude often resulted in tonic muscle contractions. In subject RA, for instance, monopolar DBS using the distal electrode as the cathode (−2 V) induced tonic muscle contractions in the face and upper limb and supplanted benefit on upper limb rigidity and bradykinesia, which prolonged movement times on the reach-and-retrieval task.

Neural correlates for improving rigidity and bradykinesia. Pallidal DBS improved rigidity using electrode contacts in GPe or GPi or even in regions outside of the GP. Comparisons between 1) model predictions of the percentage of sensorimotor GPi and GPe efferents driven at or above the stimulation frequency of 135 Hz and 2) the percent change in averaged rigidity score across all tested DBS settings showed trends with greater pallidal efferent activation paralleling less muscle rigidity in subject MA (GPe/GPi, $r^2 = 0.78/0.66$) and to a lesser extent subject RA (GPe/GPi, $r^2 = 0.32/0.27$; Fig. 6, A and B). In subject NE, there also was a clear relationship between increasing the cathodic voltage at one of the three electrode contacts located within GPi and decreased rigidity. However, for the electrode located ventral to Gpi, rigidity improved by 83% despite only driving 0.5% of Gpi and 4.5% of GPe neurons. In this animal, there was no consistent relationship for overall sensorimotor GPe or Gpi efferent activation and rigidity (GPe: $r^2 = 0.08$; GPe: $r^2 = 0.06$). In contrast, there was a consistent relationship in subject NE between activation of fibers in IC and reduction in rigidity ($r^2 = 0.71$; Fig. 6C). This relationship was also strong for subjects MA ($r^2 = 0.81$) and RA ($r^2 = 0.61$). Indeed, the most therapeutic stimulation setting for each subject was found using the electrode closest to IC (NE: contact 1; MA: contact 0; RA: contact 0).

For most electrode configurations, increased activation of any one of the neuronal pathways (GPe, GPi, and mIC) paralleled a decrease in bradykinesia with DBS (Fig. 7). In subject NE, the most consistent relationship for decreasing bradykinesia was with activation of GPe efferent projections. Interestingly, in subjects MA and RA in which the active electrodes were located within GPe, the model results indicated that bradykinesia was relieved without directly activating Gpi efferent activity. Together, these results suggest that GPe or some other fiber passing through GPe may be a therapeutic target for controlling bradykinesia. The data also showed trends between improvement in bradykinesia and activation of fibers in IC for each electrode configuration. However, the relationship was not consistent when grouping all electrode configurations together for a given subject (NE: $r^2 = 0.20$; MA: $r^2 = 0.47$; RA: $r^2 = 0.20$; Fig. 7C). Although the simulation results for rigidity indicated that there was a relative lack of spatial stimulation precision necessary to have a therapeutic effect, relieving bradykinesia with stimulation required more spatially selective targeting. Across the three subjects, the most therapeutic electrode configurations for bradykinesia

Fig. 5. Characterization of rigidity and bradykinesia in the DBS-ON state. The degree of improvement (Δ) in parkinsonian rigidity (A) and parkinsonian bradykinesia (B) with pallidal DBS depended on electrode configuration and stimulation voltage in each of the 3 subjects. Electrode configurations are represented by a letter (C, cathode; A, anode) and by a number (0 is the distal electrode, and 3 is the proximal electrode on the DBS lead). Instances of cathodic monopolar DBS used a distant ground [e.g., implantable pulse generator (IPG) can] as the anode electrode.

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were those that activated GPe and GPi efferents near the mediolateral lamina between GPe and GPi. The computational models predicted that in these instances at least 10% of pallidal neurons in both sensorimotor GPe and GPi were directly activated by the stimulation (Fig. 8). Stimulation settings that activated a greater percentage of pallidal projections near the ventral border of GPi (subject NE) or near the dorsolateral border of GPe (subjects MA and RA) resulted in less improvement in bradykinesia for stimulation amplitudes equivalent to those used with electrodes at the border between GPe and GPi.

**DISCUSSION**

High-frequency electrical stimulation targeted to the GP is known to relieve motor symptoms in medication-refractory patients with PD (Volkmann et al. 2004). Although the most commonly accepted therapeutic target in the GP has been the posteroventral sensorimotor GPi, the precise pathways involved in treating each parkinsonian motor symptom are not well-characterized. We investigated how behavioral outcome measures of bradykinesia and rigidity vary according to DBS electrode configuration and voltage settings and further how these DBS settings relate to computational model predictions of the activated pathways within GPe, GPi, and IC. The results suggest that the therapeutic effect on rigidity correlated most closely with activating a small percentage of IC fibers, whereas eliciting an optimal therapeutic effect on bradykinesia required activating a large percentage of sensorimotor GPe and GPi neurons near the mediolateral lamina.

**Mechanisms of pallidal DBS for managing parkinsonian bradykinesia.** The possibility of dissociating improvement in bradykinesia and rigidity with DBS was first suggested in a series of clinical studies with GPi-DBS patients (Bejjani et al. 1998; Krack et al. 1998; Yelnik et al. 2000). In these studies, high-frequency electrical stimulation targeted to the dorsal GPi was more effective at treating bradykinesia, whereas stimulation targeted to the ventral GPi at times worsened bradykinesia, potentially due to confounding capsular effects (Xu et al. 2011). Given the size of the DBS leads used in these studies, it is very likely that the dorsal site of stimulation was in GPe rather than dorsal GPi, which is consistent with observations in our study and previous results in humans undergoing acute stimulation in GPe (Vitek et al. 2004). The models in our study showed that improvement in bradykinesia was most significant when at least 10% of sensorimotor GPe efferent output (near the dorsomedial border with GPi) was entrained to the 135-Hz stimuli. The data also showed that bradykinesia could be relieved without direct activation of GPi efferents, suggesting that driving inhibitory axonal input into GPi is a therapeutic mechanism for improving bradykinesia with pallidal DBS (Kravitz et al. 2010; Vitek et al. 2004).

Pharmacological studies in nonhuman primates (Baron et al. 1992; Filion et al. 1991) and pallidotomy studies in humans (de Bie et al. 1999; Vitek et al. 2003) support the relationship between a reduction in GPi activity and improvement in parkinsonian bradykinesia. Electrical stimulation of GPe, using settings that improve bradykinesia, is known to have a prolonged inhibitory effect on STN and GPi activity (Vitek et al. 2012). Such modulation could be elicited through inhibition of STN-GPi neuronal activity (Kita et al. 2005), activation of GPe projections passing through GPi (Johnson and McIntyre 2008; Sato et al. 2000), and/or facilitation of the direct pathway by stimulation of striatofugal fibers synapsing on GPi neurons (Kravitz et al. 2010). Although the former and latter were not
specifically modeled in our study, they can be inferred from the fact that the axonal fiber locations driven by the most therapeutic DBS settings for bradykinesia were located at a region that would drive inhibitory afferents to GPi without significant GPi efferent stimulation (Fig. 8).

It is important to note, however, the DBS in GPe also modulates the firing pattern of GPi neuronal activity (Vitek et al. 2012). Other studies have shown that modulating the firing patterns of neurons in GPi with STN-DBS parallels improvement in bradykinesia (Hashimoto et al. 2003). Regularizing the firing pattern of activity in GP is thought to limit the pathological information content being transmitted through the pallidofugal pathway to motor thalamus and brain-stem regions (Dorval et al. 2008, 2010; Grill et al. 2004), thereby freeing downstream networks to participate in motor control more effectively. Taken together, the present study in the context of these previous studies suggests that there are likely multiple physiological mechanisms by which DBS can improve bradykinesia.

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Fig. 7. Relationships between bradykinesia and the neuronal pathways modulated by GP-DBS. The computational model was used to calculate the activation of GPe (A), GPi (B), and mIC (C) output activity at each experimentally tested DBS setting. Markers are identical to those in Fig. 6 with the addition of 4 bipolar electrode configurations (cross: cathode 0/anode 1; pentagram: cathode 1/anode 0; upward-pointing triangle: cathode 2/anode 3; right-pointing triangle: cathode 3/anode 2).

Fig. 8. Pallidal regions modulated with the most effective DBS setting for bradykinesia in each of the 3 subjects. A: volumes of activated tissue were defined according to regions in which the efferent output was entrained to the high-frequency stimulation (>80%) as shown in the coronal view from subject MA. Black boxes represent the original soma locations of activated GPe and GPi efferents. B–D: oblique perspectives showing the spatial distribution of activated regions in each subject and their localization to the medial medullary lamina. L, lateral; P, posterior.
Although our model-behavior data showed trends between improvement in bradykinesia and mIC fiber activation, the correlation was less robust than that for driving efferents from GPe and at higher levels, GPi. Nevertheless, the spread of stimulation into IC may have some aggregate effect on bradykinesia improvement (Ashby et al. 1998). Repeated transcranial magnetic stimulation over motor cortex (5 Hz, 10% below threshold for evoking contralateral muscle contractions) in patients with PD, for example, is known to reduce movement time on a peg-board test (Pascual-Leone et al. 1994a,b); whether such effects are due to direct activation of IC or induced through changes in intracortical network activity remains unclear.

Mechanisms of pallidal DBS for managing parkinsonian rigidity. The concept of different optimal target volumes for managing bradykinesia and rigidity with DBS was recently described in a computational modeling study in a cohort of STN-DBS patients with PD (Butson et al. 2011). The model simulations predicted that the optimal target volumes for treating rigidity were lateral and closer to IC than the volumetric target for treating bradykinesia. Our model predictions are consistent with these results and further show that weak activation of IC (<10%) correlates with improvement in rigidity. It is important to note that this absolute percentage reflects the excitability of the axon models, which can vary depending on the passive and active membrane properties instantiated within the fiber models (McIntyre and Grill 2002; McIntyre et al. 2002). Stimulation of pallidal projections (both GPe and GPi) in subject MA showed strong correlations with a therapeutic effect on rigidity. However, there were strong correlations between the percent activation of GPe:GPi:mIC model fibers as shown in Fig. 4, suggesting that stimulation through this lead was not able to activate one pathway over another. The lack of spatial targeting necessary to manage rigidity with DBS is consistent with clinical findings in PD patients with GPi-DBS implants (Bejjani et al. 1998; Krack et al. 1998; Yelnik et al. 2000) and a recent case study in an MPTP-treated monkey implanted in the STN with a scaled-down version of the human DBS lead (Xu et al. 2011). These studies noted that rigidity could be improved using any of the four electrode contacts on the DBS lead regardless of implantation in GPe/GPi or STN so long as the stimulation was of sufficient amplitude.

DBS amplitudes below threshold for producing contralateral muscle contractions have been implicated in the modulation of IC fiber activity (Ashby et al. 1998; Kuhn et al. 2004). In PD patients, Ashby and colleagues (1998) reported short-latency facilitation and long-latency inhibition of voluntary muscle contraction after delivering a stimulus pulse in GPi using voltage settings that at higher stimulation frequencies produced a therapeutic effect on rigidity. They observed that the distal electrode contact always had the lowest threshold for short-latency facilitation, which based on their implant trajectories would be consistent with its proximity to IC. Continuous stimulation of this tract would likely drive motoneurons and inhibit the overall population of motor cortex through antidromic signaling (Gradinaru et al. 2009; Li et al. 2007), intracortical inhibition (Johnson et al. 2009), and/or decreased motor cortex excitability (Kuhn et al. 2003). However, since the IC fiber models used in our study were constructed as nonspecific projections, it was not possible to determine the origin of the fibers (e.g., corticospinal, corticobulbar, pallidofugal, or striatofugal).

There are several possible mechanisms by which IC stimulation could improve muscle rigidity. One explanation follows the logic of limiting the amount of supraspinal drive on α-motoneurons in the spinal cord, which are known to exhibit abnormally high activity in PD patients with significant parkinsonian rigidity (Lindau et al. 1966). Indeed, IC lesions, which presumably decrease supraspinal tone on α-motoneurons, are known to have a temporary, beneficial effect on rigidity (Smith 1962). In our study, however, a small percentage of axonal fibers within IC were entrained at 135 Hz and not refractory to the high-frequency stimulation, which would seem at odds with the proposed explanation. It is possible, however, that excitation of a small percentage of fibers within IC reduces the excitability of spinal interneurons through recurrent inhibition from synchronous activation of α-motoneurons, thereby decreasing α-motoneuron activity during joint movements (Delwaide et al. 1993). An abnormal stretch reflex is also observed in PD patients (Pollock and Davis 1930), suggesting that altered Golgi tendon organ reflex activity (Burne and Lippold 1996) and/or static γ-motoneuron activity (Lee 1989) are present. Following administration of neuroleptics in animal models of parkinsonism (Ellenbroek et al. 1985; Steg 1964), γ-motoneuron activity is known to decrease. Thus it is also possible that parkinsonian rigidity could be relieved through DBS by altering the activity of static γ-motoneurons and turning down the sensitivity of the stretch reflex during joint movements (Grigg and Preston 1971). To resolve these questions, future studies should begin investigating the effects of GP-DBS or STN-DBS on brain-stem and spinal-cord activity.

The combination behavioral-modeling results from this study suggest that stimulating fibers of passage within or near GPe correlate with improving parkinsonian bradykinesia and rigidity during pallidal DBS. Improvements in parkinsonian rigidity correlated most consistently across the three subjects with spread of activation into IC, driving a small percentage of fibers within this tract (<10% on average). The most robust effect on bradykinesia resulted from stimulating a combination of sensorimotor axonal projections within the GP, specifically at the site of the medial medullary lamina. Future studies investigating motor cortex activity as well as brain-stem and spinal-cord activity may be useful for further defining differences in the mechanisms of action of DBS on parkinsonian rigidity and bradykinesia.

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DISCLOSURES

No conflicts of interest, financial or otherwise, are declared by the author(s).

AUTHOR CONTRIBUTIONS

M.D.J., C.C.M., and J.L.V. conception and design of research; M.D.J., J.Z., and D.G. performed experiments; M.D.J., J.Z., and D.G. analyzed data;
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M.D.J., J.Z., D.G., C.C.M., and J.L.V. interpreted results of experiments; M.D.J. prepared figures; M.D.J. drafted manuscript; M.D.J., J.Z., D.G., C.C.M., and J.L.V. edited and revised manuscript; M.D.J., J.Z., D.G., C.C.M., and J.L.V. approved final version of manuscript.


