Contrast-dependent phase sensitivity in V1 but not V2 of macaque visual cortex

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Cloherty SL, Ibbotson MR. Contrast-dependent phase sensitivity in V1 but not V2 of macaque visual cortex. J Neurophysiol 113: 434–444, 2015. First published October 29, 2014; doi:10.1152/jn.00539.2014.—Some neurons in early visual cortex are highly selective for the position of oriented edges in their receptive fields (simple cells), whereas others are largely position insensitive (complex cells). These characteristics are reflected in their sensitivity to the spatial phase of moving sine-wave gratings: simple cell responses oscillate at the fundamental frequency of the stimulus, whereas this is less so for complex cells. In primates, when assessed at high stimulus contrast, simple cells and complex cells are roughly equally represented in the first visual cortical area, V1, whereas in the second visual area, V2, the majority of cells are complex. Recent evidence has shown that phase sensitivity of complex cells is contrast dependent. This has led to speculation that reduced contrast may lead to changes in the spatial structure of receptive fields, perhaps due to changes in how feed-forward and recurrent signals interact. Given the substantial interconnections between V1 and V2 and recent evidence for the emergence of unique functional capacity in V2, we assess the relationship between contrast and phase sensitivity in the two brain regions. We show that a substantial proportion of complex cells in macaque V1 exhibit significant increases in phase sensitivity at low contrast, whereas this is rarely observed in V2. Our results support a degree of hierarchical processing from V1 to V2 with the differences possibly relating to the fact that V1 combines both subcortical and cortical input, whereas V2 receives input purely from cortical circuits.

IN THE PRIMATE BRAIN, visual information is processed by a network of cortical areas (Felleman and Van Essen 1991). Information from the lateral geniculate nucleus (LGN) enters the cortical network in the primary visual cortex (V1). V1 is reciprocally connected to the second visual area (V2) and other areas in the cortical network. Based on their anatomic connectivity, cortical areas V1 and V2 are often considered sequential stages in a functional hierarchy (e.g., Lund 1988). Whereas V1 receives input from the LGN, V2 receives the majority of its input from V1. However, both areas are modulated by cortical connections. In both primate brain areas, most neurons are selective for the orientation and the spatial and temporal frequency of moving gratings presented within their excitatory receptive fields (Foster et al. 1985), as is also the case in many other mammalian species (e.g., cat: Hubel and Wiesel 1962, rodent: Girman et al. 1999; marsupial: Ibbotson and Mark 2003). Some cortical neurons are selective for the spatial phase of the gratings (simple cells), whereas others (complex cells) are considered phase invariant (Movshon et al. 1978a,b; but also see Hietanen et al. 2013). In addition to their selectivity for visual stimulus attributes, neural responses are modulated by both spatial and temporal stimulus context. Responses to stimuli presented within the excitatory receptive field of a neuron may be modulated by stimuli presented outside of their receptive field (Sengpiel et al. 1997) or by previously presented stimuli (Ohzawa et al. 1982, 1985). Also, selectivity for size and spatial frequency of neurons in V1 is dependent on stimulus contrast (Kapadia et al. 1999; Sceniak et al. 1999, 2002; Shushruth et al. 2009). A proportion of complex cells in primary visual cortex increase their phase sensitivity at low contrast following contrast adaptation and in the presence of stimuli presented within the inhibitory surround of their receptive field (cat: Bardy et al. 2006; Crowder et al. 2007; Romo et al. 2011; van Kleeft et al. 2010; monkey: Durand et al. 2012; Henry and Hawken 2013).

Here, for the first time, we investigate the effect of stimulus contrast on the observed phase sensitivity of complex cells in primate area V2 and compare it with V1 using a novel analysis technique that controls for changes in spike count. This affords an informative comparison of two processing stages. Responses in V1 reflect cortically modulated input from the LGN, whereas responses in V2 reflect cortically modulated cortical input. We show that a proportion of complex cells in V1 exhibit increased phase sensitivity at low stimulus contrast. In most cases, this increase is most prominent at threshold contrast, which we defined as the lowest contrast evoking a just-detectable response determined using a receiver operating characteristic (ROC) analysis. By investigating neuronal responses at threshold, we reveal changes in phase sensitivity that emerge at the limits of spatial and temporal summation. Although our data demonstrate dynamic phase sensitivity in a significant proportion of neurons in V1, we find that phase sensitivity of neurons in V2 is largely contrast invariant. This suggests that in primates the cortical networks underlying responses in V2 summate information in a different way from the combined LGN and cortical networks underlying responses in V1.

MATERIALS AND METHODS

Electrophysiology. We made extracellular recordings of spiking responses from 300 well-isolated single units in V1 (n = 166) and V2...
(n = 134) of 6 anesthetized macaque monkeys (5 Macaca fascicularis, 4.3–4.7 kg; 1 M. nemestrina, 8 kg). All surgical and experimental procedures were approved by the Animal Welfare Committee at New York University and conformed to the National Institutes of Health Guide for the Care and Use of Laboratory Animals. Monkeys were prepared for acute electrophysiological recordings using procedures identical to those described in Cavanaugh et al. (2002). A craniotomy was performed over V1, centered 10 mm posterior to interaural zero and 12 mm lateral to the midline. Extracellular recordings were made with quartz/platinum-tungsten microelec-

trodes (Thomas Recording), which penetrated the surface of V1 2–4 mm behind the lunate sulcus. Electrodes were advanced in the rostral direction at an angle of 20° from vertical within a parasagittal plane 10–13 mm lateral to the midline. Electrode penetrations traversed the gray matter in V1 followed by a region of white matter (characterized by an absence of spiking activity) before entering the gray matter in V2 on the posterior bank of the lunate sulcus (typically 2,500–3,500 μm from the start of the penetration on the surface of V1). Recorded units were ascribed to either V1 or V2 on the basis of their position relative to the surface of V1, the relationship with the transitions between gray and white matter, and by tracking changes in receptive field topography along the electrode track. Our electrode penetrations were such that cells encountered in V1 and V2 had receptive fields of similar eccentricity; receptive fields for most cells were between 2 and 5° eccentricity. For the purpose of assessing the laminar distribution of recorded cells, the relative cortical depth for each recorded cell was calculated as a fraction of the distance along the electrode track.

Signals from the microelectrodes were amplified, band-pass filtered (300 Hz to 10 kHz), and sampled with 16-bit precision at a rate of 25 kHz. Single units were isolated online using dual-window time-amplitude discrimination software (Expo; P. Lennie, University of Rochester). Spike times were saved with a temporal resolution of 0.1 ms.

Visual stimuli and data acquisition. Visual stimuli were generated by an Apple Macintosh computer running Expo. Stimuli were pre-

sented on a calibrated EIZO FlexScan T966 CRT monitor at a resolution of 1,280 × 960 pixels (width × height) and a refresh rate of 120 Hz. The monitor was viewed by the animal from a distance of 114 cm, subtending 20 × 15° of visual angle. The mean luminance of the monitor was 31.2 cd/m². Stimuli were presented monocularly on a mean gray background and consisted of luminance-modulated sine-wave gratings windowed by a soft-edged circular aperture centered on the receptive field of the dominant eye. For each cell, we first determined the direction, spatial frequency, temporal frequency, and size of the grating that evoked the maximal response. We then studied the response of each cell to optimal moving sine-wave gratings of 10 different Michelson contrasts equally spaced on a log scale between 0.01 and 1.0. Gratings and a blank (mean gray) condition were presented for 1 s, interleaved in block pseudorandom order, with no interstimulus interval. For each cell, the stimulus was repeated as often as was practical (median 20 times) depending on the stability of the isolation of the cell.

Analysis of neuronal responses. For each cell, we computed the firing rate for each stimulus condition, including the blank condition, within an analysis window equal to the stimulus duration (1 s). We chose the onset of the analysis window to maximize the variance of the mean firing rate across all stimulus conditions (Smith et al. 2005). For each trial, we discarded the response to the first cycle of the stimulus to remove the influence of onset transients (Bonhoeffer and Mark 1996) and then cycle-averaged the responses to each stimulus condition across trials. We estimated the baseline spontaneous activity of each cell as the mean spike count during presentation of the blank condition. At each stimulus contrast, we quantified the phase sensitivity of the cell by Fourier analysis of the cycle-averaged spiking response. Specifically, we calculated the relative modulation, \( F_1/F_0 \), of the responses as the amplitude of the Fourier coefficient at the fundamental frequency of the grating stimulus (\( F_1 \)) divided by the mean response (\( F_0 \)) after subtraction of the estimated baseline spontaneous activity. We classified cells as simple or complex according to the observed \( F_1/F_0 \) at maximum contrast (Dean 1981; Movshon et al. 1978a,b; Skottun et al. 1991).

We compared relative modulation of the observed responses at high and low stimulus contrast. For each cell, the high-contrast condition was defined as the stimulus contrast that evoked the maximal response. For most cells, this was 100% contrast. For 2 cells (1 in each of V1 and V2), the maximal response was observed at 60% contrast. The low-contrast condition was defined as the lowest stimulus contrast tested that evoked a response significantly above the baseline spontaneous rate of the cell. Owing to differences in contrast gain, the low-contrast condition was different for each cell. We determined the appropriate low-contrast condition for each cell based on a ROC analysis (Green and Swets 1966; Tolhurst et al. 1983). Specifically, we compared the observed spike counts for each stimulus contrast tested with those observed during presentation of the blank condition. We quantified the discriminability of the response to each stimulus contrast as the area under the ROC. This represents the probability that an ideal observer would correctly distinguish the grating of a given contrast from the blank stimulus. To assess the significance of the area under the observed ROC at each stimulus contrast, we performed a permutation test (Efron and Tibshirani 1993). We sampled without replacement from the available pool of responses, without regard to the stimulus that was presented (be it the blank or the grating stimulus), and calculated the resulting area under the ROC. This sampling procedure was repeated 10,000 times, producing a null distribution for the area under the ROC. The response to a given stimulus contrast was deemed significantly above the baseline rate if the area under the observed ROC exceeded 99% of the null distribution (i.e., \( P < 0.01 \)).

Expected increase in \( F_1/F_0 \) with reduced spike count. Quantifying phase sensitivity by Fourier analysis of spiking responses is sensitive to the number of spikes recorded (Crowder et al. 2007; Hietanen et al. 2013). To account for the increase in \( F_1/F_0 \) due to the reduction in the number of spikes as stimulus contrast was reduced, we compared the observed \( F_1/F_0 \) of each cell with an empirical distribution of \( F_1/F_0 \) derived from a model complex cell. The model cell produces responses containing \( n \) spikes over a response interval \( T \), which we define to be one cycle of an optimal sine-wave grating. Spike arrival times, \( t \in [\pi, \pi] \), are assumed to be independent, identically distributed random variables drawn from a raised cosine distribution defined by:

\[
f(t; A, B) = \frac{1}{\pi} \left[ 1 + \cos(\pi (t - B)) \right] \quad B - \pi \leq t < B + \pi \quad (1)
\]

where \( 0 \leq A \leq 1 \) defines the assumed true or asymptotic \( F_1/F_0 \) (i.e., the expected value of \( F_1/F_0 \) as \( n \to \infty \), denoted as \( (F_1/F_0)_\infty \)), and \( B \) defines the position of the distribution. The standard raised cosine distribution corresponds to \( A = 1 \) and \( B = 0 \). For \( A = 0 \), Eq. 1 reduces to the uniform distribution, corresponding to an ideal phase-invariant complex cell. To simulate responses with a given asymptotic \( (F_1/F_0)_\infty \), we set \( A = (F_1/F_0)_\infty \) and \( B = 0 \).

We determined the appropriate asymptotic \( (F_1/F_0)_\infty \) for each cell by maximizing the likelihood of the data observed. Specifically, for each cell, we computed the log likelihood \( L \) of the data for a given asymptotic \( F_1/F_0 \) as follows:

\[
\log L = \log \prod_i f(A_j, A) \quad (2)
\]

where \( A_j \) is the relative modulation (i.e., \( F_1/F_0 \)) of the cell based on the observed response containing \( n \) spikes, \( A \) is the specified asymptotic level of response modulation for the model (Eq. 1), and \( j \) is an index over stimulus contrast (here indexing the stimulus contrast producing the maximal response).

After choosing the asymptotic \( F_1/F_0 \) for the model to maximize the likelihood of the data observed at maximum contrast, we computed

\[
\text{ Equation (1) }
\]

\[
\text{ Equation (2) }
\]
distributions of $F_1/F_0$, at spike counts ($n$) corresponding to the number of spikes recorded at each of the lower stimulus contrasts tested for each cell. From these distributions, we calculated 99% confidence limits for the increase in $F_1/F_0$, which might be expected simply due to the reduction in the number of spikes observed. For the increase in $F_1/F_0$ observed for a given cell at low contrast to be considered significant, it must exceed the increase in $F_1/F_0$ expected simply due to the reduction in the number of spikes, i.e., it must exceed the 99% confidence limit of the corresponding empirical distribution.

RESULTS

We made extracellular recordings of spiking responses from neurons in V1 and V2 of six anesthetized monkeys. Specifically, we quantified the phase sensitivity of the response of each cell to optimal moving sine-wave gratings over a range of stimulus contrasts.

Spiking responses from an example complex cell in macaque V1 are shown in Fig. 1A for a range of stimulus contrasts. When tested at 100% contrast (Fig. 1A, right), this cell exhibits a moderate level of response modulation ($F_1/F_0 = 0.44$). Weak modulation of spiking responses to optimal moving sine-wave gratings is characteristic of many complex cells (Hietanen et al. 2013; Ibbotson et al. 2005). As contrast is reduced (Fig. 1A, middle and left panels), the relative contribution of the modulated component of the response to the overall response of the cell increases. The response of this cell was indistinguishable from the spontaneous background for stimulus contrasts below 8%. Figure 1B shows the amplitude of the mean response ($F_0$) and first harmonic Fourier component ($F_1$) for this cell plotted against stimulus contrast. The mean component of the response decreases monotonically with decreasing stimulus contrast, whereas the modulated response component ($F_1$) peaks at moderate stimulus contrast (36%). Despite the reduction in overall response amplitude, the relative modulation ($F_1/F_0$) of the response increases monotonically with decreasing stimulus contrast (Fig. 1C).

Fourier analysis of spiking responses is sensitive to the number of spikes observed: $F_1/F_0$ is expected to increase as the number of spikes observed is reduced (Hietanen et al. 2013). Any increase in $F_1/F_0$ as contrast is reduced is therefore confounded by the concomitant reduction in the number of spikes. In assessing the magnitude of any observed change in $F_1/F_0$, it is therefore necessary to control for the effect of changes in spike count. Figure 2 illustrates the relationship between expected $F_1/F_0$ and spike count derived from the model complex cell for a range of asymptotic $F_1/F_0$ values (red curves; the asymptotic $F_1/F_0$ value giving rise to each curve is indicated in red on the right of Fig. 2A). For low spike counts, the expected value of $F_1/F_0$, denoted by $\langle F_1/F_0 \rangle$, may lie far from the specified asymptotic $F_1/F_0$ value. The exact value of $\langle F_1/F_0 \rangle$ depends on the number of spikes ($n$). As $n$ approaches the lower bound of 1 spike, $\langle F_1/F_0 \rangle$ approaches 2 (all of the curves in Fig. 2A converge to $F_1/F_0 = 2$ at $n = 1$).

Consider again the example cell shown in Fig. 1. For this cell, we recorded a total of 1,130 spikes across all repeats at a stimulus contrast of 100% and estimated $F_1/F_0 = 0.44$ (Fig. 1C). Figure 2B shows the likelihood of the observed data as a function of the assumed asymptotic $F_1/F_0$ value (leftmost curve). The likelihood peaks at $F_1/F_0 = 0.44$. This is consistent with the value estimated from the data, as expected given the relatively large number of spikes recorded for this cell at 100% contrast and the shallow slope of the relationships illustrated in Fig. 2A. The relationship between $F_1/F_0$ and spike count for an asymptotic $F_1/F_0 = 0.44$ is shown by the thick red line in Fig. 2A. Figure 2C shows empirical distributions of $F_1/F_0$ for 50, 100, and 500 spikes for the model complex cell with an asymptotic $F_1/F_0 = 0.44$. As the number of spikes increases, the mean of the empirical distribution (i.e., $\langle F_1/F_0 \rangle$, indicated by the solid red lines in Fig. 2C) approaches the specified asymptotic $F_1/F_0$ value and the spread of the distribution decreases (broken lines indicate the 99% confidence limit for each distribution).

For comparison of the model with the experimental data from the example cell, Fig. 2A shows the observed $F_1/F_0$ for the example cell for stimulus contrasts between 8 and 100%.
illustrate the increased bias and uncertainty of estimating confidence limit is indicated by the broken red line. These distributions are the same data points as shown in Fig. 1C, plotted against their corresponding spike counts. For further comparison of the model with the observed data, \( F_1/F_0 \) for the complex cell model is also plotted against stimulus contrast in Fig. 1C (solid red line) together with the corresponding 99% confidence limits (broken red line). Clearly, Figs. 1 and 2 illustrate that for the example cell the increase in \( F_1/F_0 \) observed as stimulus contrast is reduced far exceeds that expected due to the reduction in spike count alone.

For even moderate stimulus contrasts, the observed \( F_1/F_0 \) lies well above the 99% confidence limit (Fig. 1C). Figure 2B also shows the likelihood of the data observed at each stimulus contrast (and corresponding spike count) as functions of the assumed asymptotic \( F_1/F_0 \) value. The peaks of these curves move to the right as contrast is reduced. This shift reveals the failure of a static model (i.e., a single asymptotic \( F_1/F_0 \)) to explain the level of relative modulation observed at all stimulus contrasts, suggesting a change in the operating regime (i.e., the asymptotic \( F_1/F_0 \)) of the cell as contrast is reduced.

To quantify the change in \( F_1/F_0 \) with contrast across our cell populations in V1 and V2, we compared the \( F_1/F_0 \) observed at high contrast with that observed at stimulus contrast for each cell. Owing to differences in contrast gain between cells, the low-contrast condition was necessarily different for each cell. We determined the appropriate low-contrast condition (i.e., threshold contrast) for each cell based on a ROC analysis. Figure 3A shows ROCs for the example cell corresponding to each of the stimulus contrasts tested. Spiking responses of this cell were not significantly different from the spontaneous background for stimulus contrasts below 8% (permutation test, \( P > 0.01 \); ROCs shown in gray). Figure 3, B and C, shows the distribution of threshold contrast for cells in V1 and V2, respectively (colored bars, complex cells; gray bars, simple cells). Both of these distributions deviate from normal (Lilliefors' goodness-of-fit test, \( P > 0.05 \)). We found no significant difference between these 2 distributions (2-sample Kolmogorov-Smirnov goodness-of-fit test, \( P = 0.78 \)). Figure 3, D and E, shows corresponding distributions of the area under the ROCs for all cells in V1 and V2, respectively. Comparison of the distributions in Fig. 3, B–E, reveals no systematic difference between the stimuli or the detectability of responses used to assess phase sensitivity in V1 and V2.

Figure 4A shows \( F_1/F_0 \) at the lowest contrast that produced a significant response (based on the ROC analysis) plotted against \( F_1/F_0 \) at high contrast for 166 cells from V1. The median \( F_1/F_0 \) for our complex cell population in V1 increased from 0.33 at high contrast to 0.65 at threshold contrasts. Individually, 46/105 (44%) of the complex cells we recorded in V1 exhibited a significant increase in \( F_1/F_0 \), i.e., an increase that exceeds their corresponding 99% confidence limit and cannot be attributed simply to a reduction in the number of spikes observed. These cells are indicated by the green symbols in Fig. 4A. Figure 4B shows comparable data for 134 cells from V2. We observed a much smaller increase in median \( F_1/F_0 \) for complex cells in V2 as contrast was reduced (0.33 at threshold contrasts compared with 0.29 at high contrast). Notably, the number of complex cells for which the observed increase in \( F_1/F_0 \) could not be attributed to a reduction in the number of spikes observed was very small in V2 (9/122 cells, 7%; blue symbols in Fig. 4B).
We quantified the change in $F_i/F_0$ on a cell-by-cell basis for all cells in V1 and V2. Simple cells in both V1 and V2 showed no consistent change in $F_i/F_0$ with contrast (V1: 0.03, 2-sided Wilcoxon signed-rank test, $P = 0.37$; V2: −0.15, 2-sided Wilcoxon signed-rank test, $P = 0.13$). The situation was very different for complex cells. Figure 4, C and D, shows distributions of the change in $F_i/F_0$ at threshold contrast compared with high contrast for complex cells in V1 and V2, respectively. The differences in these distributions are very clear. Complex cells in V1 showed a significant increase in $F_i/F_0$ at threshold contrasts with a median change across all complex cells in V1 of 0.32 (2-sided Wilcoxon signed-rank test, $P < 0.001$; Fig. 4C). In contrast, complex cells in V2 showed a much smaller increase in $F_i/F_0$ at threshold contrasts (median change 0.08; 2-sided Wilcoxon signed-rank test, $P < 0.001$; Fig. 4D). When assessed individually, a subset of complex cells in both V1 and V2 exhibited a significant increase in $F_i/F_0$ at threshold contrast (colored symbols in Fig. 4, A and B). The distributions of the change in $F_i/F_0$ for those cells is shown by the colored bars in Fig. 4, C and D. Among those cells, the magnitude of the change was comparable in V1 and V2 (median increase of 0.64 and 0.57, respectively; Wilcoxon rank-sum test, $P = 0.92$). However, as already noted, the proportion of complex cells in V2 exhibiting a significant increase in $F_i/F_0$ at threshold contrast was very low (only 7% for V2 vs. 44% for V1).

Although the distributions of the change in $F_i/F_0$ for complex cells in V1 and V2 (Fig. 4, C and D) show the absolute change in relative modulation of observed responses, this difference does not account for the influence of reduced spike count at low contrast. For each cell, we quantified the change in $F_i/F_0$ not attributable to a reduction in spike count by subtracting $F_i/F_0$ given by the model from $F_i/F_0$ observed at threshold contrast. If the $F_i/F_0$ ratio observed at threshold contrast was due to limited spike count, we would expect this difference to be distributed around 0. The distributions of this metric for complex cells in V1 and V2 are shown in Fig. 4, E and F, respectively. Across all complex cells in V1, this metric was significantly greater than 0 (median 0.24; 2-sided Wilcoxon signed-rank test, $P < 0.001$; Fig. 4E). This reveals that on average, complex cells in V1 show greater relative modulation of their responses at low contrast than would be expected due to reduced spike count. This is not the case in V2. The median of the distribution for V2 is not significantly different from 0 (median −0.005, 2-sided Wilcoxon signed-rank test, $P = 0.99$; Fig. 4F), suggesting that in V2 the relative modulation of responses at low contrast is adequately explained by the reduced spike count.

The colored bars in Fig. 4, E and F, show the distributions for the subset of complex cells in V1 and V2 that showed a significant increase in $F_i/F_0$ when assessed individually. The medians of the distributions for V1 and V2 are comparable (V1, 0.53; V2, 0.52; Wilcoxon rank-sum test, $P = 0.99$) and significantly greater than 0 (V1, $P < 0.001$; V2, $P = 0.003$; Wilcoxon signed-rank test).

To allow comparison of the absolute response rate for our cells recorded in V1 and V2, Fig. 5 shows distributions of the $F_0$ and $F_i$ response components recorded at maximum contrast for all cells. Figure 5, A and B, shows the distributions of $F_0$ and $F_i$, respectively, for cells recorded in V1, whereas Fig. 5, C and D, shows comparable distributions for cells recorded in V2 (colored bars, complex cells; gray bars, simple cells). For the majority of complex cells in both V1 and V2, the $F_0$ response component had amplitudes between 0 and 70 spikes per second. A small proportion of complex cells in V1 had $F_0$ amplitudes >70 spikes per second. In both V1 and V2, the $F_i$ response components had amplitudes between 0 and 30 spikes per second. Altogether, our populations of complex cells recorded in V1 and V2 generated responses with comparable overall spike rates, and it is unlikely that the small differences
in absolute response rate could account for the dramatic difference we observe between the 2 cell populations.

Laminar organization. To investigate the laminar distribution of our cells, Fig. 6, A and B, shows the relative cortical depth for all recorded cells in V1 and V2, respectively, plotted against the relative modulation of their responses at high contrast. In each case, the running median $F_1/F_0$ computed with a window size of 100 μm is shown superimposed (solid black line). For our population of cells from V1 (Fig. 6A), the running median $F_1/F_0$ exhibits a characteristic pattern of peaks and troughs that correlates well with that previously reported for macaque V1 (Ringach et al. 2002; shown by the dashed black line in Fig. 6A). The correlation between the running median $F_1/F_0$ for our data and that reported by Ringach et al. (2002) is extremely high ($r = 0.795$, $P < 0.001$). Green symbols in Fig. 6A indicate those complex cells that exhibit a significant increase in relative modulation of their responses at threshold contrast. These cells were found in all cortical layers.

Figure 6C shows the change in $F_1/F_0$ not attributable to a reduction in observed spike count for all complex cells recorded in V1. This is the same metric as shown in Fig. 4E, plotted here at the relative cortical depth for each cell. The running median, computed with a window size of 100 μm, is shown superimposed (solid black line). To identify regions in which the median change in $F_1/F_0$ is greater than expected due to a reduction in observed spike count, we performed a bootstrap hypothesis test (Efron and Tibshirani 1993). Specifically, we sampled with replacement from the total pool of complex cells recorded in V1 and computed the running median of the change in $F_1/F_0$ that is not attributable to a reduction in spike count. At each cortical depth, the observed median change in $F_1/F_0$ was found to be significantly different from 0 (median $-0.0595$; 2-sided Wilcoxon signed-rank test, $P = 0.001$). In contrast, the median of the distribution for complex cells in V2 is not significantly different from 0 (median $-0.0050$; 2-sided Wilcoxon signed-rank test, $P = 0.99$), demonstrating that relative modulation of responses of complex cells in V2 is consistent with that expected due to reduced spike count.
in C reduction in observed spike count for all complex cells re-
count. The observed changes in relative modulation at low
spiking responses could not be ascribed solely to low spike
tical bounds outside which any observed modulation of the
purely as a result of the reduction in spike count (Hietanen
2007). However, calculating the relative modulation of
relative modulation (\(F_1/F_0\)) of cycle-averaged
responses at threshold and at twice threshold contrast. They
found that 32% of complex cells showed a significant increase
in relative modulation of their responses at threshold contrast.
This proportion reduced to 17% when assessing responses at
twice threshold. Henry and Hawken (2013) concluded that
although on average complex cells in their population exhibit
an increase in relative modulation of their response at threshold
contrast, this was largely a consequence of low firing rates and
the finite data available. Although this is true for the majority
of their cell population, it is not true for almost a third of cells
(32%), which they report exhibited a significant increase in
\(F_1/F_0\) at threshold contrast, even after specifically accounting
for the effect of reduced spike count. In our recordings,
we assessed the responses of V1 and V2 neurons at just-detectable
stimulus contrasts. At these contrasts, we found that an even
higher proportion (44%) of complex cells in V1 showed a
significant increase in relative modulation of their responses.
However, the results from V2 were drastically different. Only
7% of complex cells in V2 showed a significant increase in
relative modulation of their responses even at just-detectable
stimulus contrasts. Our results reveal interesting changes in
the summation properties of cortical neurons at just-detectable
contrasts. In our view, it seems likely that the observed effects
are a consequence of the mechanism by which complex cell
receptive fields are formed. If this is the case, it is apparent that
the formation of complex cell receptive fields is different in V1
and V2.

Laminar organization. In V1, the axons from the dorsal
LGN terminate primarily in layer 4C (Lund 1988). Some LGN
axons also provide input to layer 6 (Fitzpatrick et al. 1985;
Hendrickson et al. 1978). Most other layers receive minor
direct input from the LGN with two exceptions: layers 4B and
5 receive no direct thalamic input (Fitzpatrick et al. 1985; Lund
1988).

The laminar organization of V1 is reflected in the receptive
field and response properties of V1 neurons (Gilbert 1977).
Notably, simple and complex cells are nonuniformly distrib-
uted with respect to cortical layer. Ringach et al. (2002)
showed that the median modulation ratio (\(F_1/F_0\)) for a large
sample of V1 neurons peaked at \(-1.4\) in the middle of layer 4C
(Fig. 6A), reflecting a predominance of simple cells in this
geniculocipient layer. They also reported an almost equal
distribution of simple and complex cells in layer 6 such that
the median \(F_1/F_0\) there was close to unity. These findings demon-
strate that simple cells and complex cells exhibiting substantial
relative modulation of their responses tend to reside in close
proximity to the termination zones of the dominant geniculate
inputs. Conversely, the median \(F_1/F_0\) was reportedly well
below unity in all other layers (Ringach et al. 2002). Before
assessing the laminar distribution of cells in our data set, we

**DISCUSSION**

Investigations of neuronal responses in geniculocrecipient
regions of cat primary visual cortex have shown that reduc-
ing stimulus contrast leads to significant increases in the
relative modulation (\(F_1/F_0\)) of responses to moving gratings
among complex cells but not simple cells (Crowder et al.
2007). However, calculating the relative modulation of
spiking responses is problematic at low contrast due to the
low spike rates encountered: relative modulation increases
purely as a result of the reduction in spike count (Hietanen
et al. 2013; van Kleeft et al. 2010). Therefore, Crowder and
colleagues (2007) performed simulations to establish statis-
tical bounds outside which any observed modulation of the
spiking responses could not be ascribed solely to low spike
count. The observed changes in relative modulation at low

\[ \text{Fig. 5. Distribution of } F_0 \text{ and } F_1 \text{ in V1 and V2. A and B: distributions of } F_0 \text{ and } F_1, \text{ respectively, for all cells recorded in V1. C and D: comparable distributions of } F_0 \text{ and } F_1 \text{ for all cells recorded in V2. In all cases, colored bars show the distributions for complex cells, whereas gray bars show the distributions for simple cells.} \]
We found very few complex cells in V2 that exhibited significant phase sensitivity among complex cells in layer 4C and 6, though they reported an overrepresentation of contrast-dependent phase sensitivity in macaque V1. Al-though they too, found cells of this type in all layers. As proposed and modeled previously (Crowder et al. 2007; van Kleef et al. 2010), if this were the case, the complex inputs to complex cells in layers 3B, 4B, 4C, and 6 have high contrast thresholds, whereas others have low contrast thresholds, reducing contrast to just-detectable levels would greatly reduce the influence of those inputs with high contrast thresholds. As proposed and modeled previously (Crowder et al. 2007; van Kleef et al. 2010), if this were the case, the complex connections to V2 from V1 terminate primarily in layers 3B and 4 with less dense terminals also found in layer 3A and the boundary between layers 5 and 6 (Lund et al. 1981). We found very few complex cells in V2 that exhibited significant increases in their phase sensitivity at low contrast. Nevertheless, in contrast to V1, where such cells were found in all layers, those cells we did find in V2 were seemingly clustered in the mid- to lower layers. This apparent clustering is unlikely to have arisen by chance (bootstrap, \( P < 0.05 \)). We therefore tentatively suggest that in area V2 those few complex cells that exhibit a significant increase in phase sensitivity at low contrast are found in layers that receive afferent input from V1 (putatively layers 4 and 5).

**Mechanisms.** Hubel and Wiesel (1962) proposed a hierarchical model for the formation of cortical receptive fields in which V1 simple cells combine input from the geniculate, engendering them with tuning for orientation and spatial frequency, and V1 complex cells combine input from spatially offset simple cells to generate phase-invariant responses. The laminar organization of area V1, as described in the previous section, lends some qualitative support to a hierarchical model for cortical processing. If some of the geniculate or simple cell inputs to complex cells in layers 3B, 4B, 4C, and 6 have high contrast thresholds, whereas others have low contrast thresholds, reducing contrast to just-detectable levels would greatly reduce the influence of those inputs with high contrast thresholds. As proposed and modeled previously (Crowder et al. 2007; van Kleef et al. 2010), if this were the case, the complex...
cells would become more phase sensitive as contrast is reduced. A similar hierarchical circuit to that proposed to link simple and complex cells in V1 has also been described for connections between cortical areas V1 and V2 (El-Shamyleh et al. 2013). From 59 neurons shown to provide direct input from V1 to V2, ~60% were strongly phase sensitive (i.e., simple). This suggests that complex cells in V1 receive input from a high proportion of V1 simple cells in addition to complex cells, challenging the notion that V1 input to V2 is dominated by complex like spatiotemporal filters (El-Shamyleh et al. 2013). In light of this, it would appear that the V1 input to V2 is similar to the input to complex cells within V1, i.e., a combination of both simple and complex like filters. Despite this similarity in their input, neurons in V2 are thought to combine input from V1 to generate sophisticated feature selectivity not encoded in V1 (Freeman et al. 2013). On this basis, complex cells in V2 are not simply functional replicas of complex cells in V1. Similarly, our results demonstrate that phase sensitivity of complex cells in V2 differs substantially from that in V1. Whereas a substantial proportion of complex cells in V1 exhibit evidence of underlying phase sensitive input when driven near threshold, the same is very rare in V2. It would appear that the mechanisms by which complex cells in V2 combine inputs from simple cells in V1 eliminate the phase sensitivity of those inputs such that it cannot be revealed by simple stimulus manipulations such as reducing contrast. This suggests that distinctly different neural mechanisms for phase averaging and summation are at work for complex cells in V1 and V2.

Although an elegant concept, the hierarchical model is based entirely on feedforward connections, and there is sufficient diversity in V1 complex cell responses that one model cannot explain all effects (Henry 1977; Spitzer and Hochstein 1988). Driven by evidence showing enormous intracortical connectivity (Peters et al. 1994), computational models suggest that simple and complex receptive fields can be created by adjusting the strength of recurrent intracortical connections (e.g., Chance et al. 1999; Tao et al. 2004; Wieland et al. 2001; Zhu et al. 2009). Such models also overcome problems associated with schemes based only on feedforward connections. For example, the existence of largely linear simple cell receptive fields is difficult to explain based on feedforward connections because of the nonlinearities inherent in their geniculate inputs. However, phase averaging and strong nonlinear inhibition via intracortical connections can effectively “linearize” simple cell responses in recurrent models of cortex (Wieland et al. 2001). Given that our results show that some complex cell receptive fields in V1 become more linear at low contrast, we suggest that contrast-dependent changes in intracortical connectivity could, at least in part, explain our findings.

The presence of many complex cells in V1 that do not show significant changes in phase sensitivity suggests that the feedforward convergence of simple cells onto complex cells is likely only one mechanism realized in V1. Indeed, many others have been proposed (for review, see Priebe and Ferster 2012), and there is experimental evidence for a diversity of mechanisms: inactivation of layer A in the LGN deactivates layer 4 simple cells but not all layer 2/3 complex cells (Malpeli 1983; Martinez and Alonso 2001; see also Calloway 2001), some complex cells have been shown to receive direct LGN input (Bullier and Henry 1979; Heggelund 1981; Martin and Whitteridge 1984), and many simple cells may receive excitatory input from complex cells (Rust et al. 2005). Based on our experiments, we cannot suggest a single model to explain how or why relative modulation of complex cell responses increases at low stimulus contrast in V1. However, our observations reveal that significant changes do occur, warranting further investigation (for an extensive discussion of possible models, see van Klee et al. 2010). The fact that V2 shows little change in phase sensitivity suggests that its strictly intracortical connections and increased spatial summation negate any contrast-dependent changes otherwise inherited from V1.

Simple cells in V1 have spatially segregated subregions within their receptive fields that are sensitive to luminance increments (bright subregions) or decrements (dark subregions). For complex cells in V1, this spatial segregation is either less obvious or absent (Hubel and Wiesel 1962; Mata and Ringer 2005). It is possible that the increase in response modulation observed in V1 and V2 complex cells at low stimulus contrast reflects a change in the spatial structure of the receptive fields of the cells. Two studies of receptive fields in macaque cortex support this hypothesis. Using reverse correlation of responses to dynamic noise stimuli, Mata and Ringach (2005) quantified the degree of overlap between bright and dark subregions within the receptive fields and compared the degree of subregion overlap with the observed relative modulation of responses to moving gratings. They showed that measures of subregion overlap are significantly correlated with the relative modulation of responses to moving gratings. Importantly, they also showed that small changes in the relative gain of the bright and dark subregions of the receptive fields can lead to reclassification of cells from simple to complex. These findings suggest that the increase in relative modulation we observe at threshold contrasts could reflect a change in the spatial structure of the receptive fields: either a reduction in subregion overlap or a change in the relative gain of the bright and dark subregions.

Durand et al. (2012) conducted experiments in primate V1 to investigate how the spatial receptive field properties of neurons change as contrast is reduced. They found that there were small but significant reductions in receptive field subregion overlap as contrast was reduced from high to medium values. Although the reduction in overlap was small (no complex cells were reclassified as simple), the finding offers some support for a mechanism in which the increase in phase sensitivity observed by us at lower contrasts may be related to changes in the spatial structure of receptive fields. However, differences in methodology need to be considered carefully. Using stimuli consisting of briefly presented oriented bars, Durand et al. (2012) also noted that receptive field width was decreased significantly as contrast was reduced. However, when using moving gratings, they found that receptive field area increased as contrast was reduced (the latter being consistent with a previous report by Sceniak et al. 1999). Clearly, the way that stimulus contrast influences receptive field structure is somewhat dependent on other stimulus properties. In our experiment, we used optimal moving gratings. Therefore, direct comparison with the observations of Durand et al. (2012) and any interpretation regarding possible mechanisms may not be appropriate.
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DISCLOSURES

No conflicts of interest, financial or otherwise, are declared by the author(s).

AUTHOR CONTRIBUTIONS


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