Sensory Input Directs Spatial and Temporal Plasticity in Primary Auditory Cortex

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INTRODUCTION

Experiments conducted over the last 20 years have documented that cortical representations are continually shaped by experience (Buonomano and Merzenich 1998; Edeline 1999; Gilbert 1998; Katz and Shatz 1996; Merzenich et al. 1996; Singer 1995). Numerous studies have suggested that experience-dependent plasticity provides the neural basis for the substantial improvement in performance that typically develops with extended practice on simple discrimination tasks. In animal models of learning, both spatially and temporally based tasks lead to progressive improvements in behavioral performance; however, the form of neural plasticity that underlies these improvements can be quite distinct. For example, receptive fields in the somatosensory cortex of New World monkeys are substantially increased by training on temporal judgments, while fine tactile manipulations decrease receptive-field sizes (Jenkins et al. 1990; Recanzone et al. 1992c; Wang et al. 1995). A more complete description of the rules that transform sensory experience into useful changes in the distributed cortical representation is needed 1) to relate the cellular rules of synaptic plasticity to observed experience-dependent plasticity in large populations of neurons, and 2) to clarify how these rules contribute to both the flexibility and reliability of the integrated operation of cell assemblies operating across the cortex.

Although it is clear that the degree and direction of cortical plasticity depends on the behavioral paradigm used to produce it, it is not yet clear what specific aspects of these different experiences are responsible for the distinct forms of observed cortical reorganizations. Studies of experience-dependent plasticity often differ in a number of parameters likely to be important for determining the form of plasticity, including modality, behavioral response, task difficulty, task goal, motivation, duration of training, background stimuli, and species (Bakin et al. 1992, 1996; Buonomano and Merzenich 1998;…

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Address for reprint requests: M. P. Kilgard, Neuroscience Program, School of Human Development, GR 41, University of Texas at Dallas, Richardson, TX 75083-0688 (E-mail: kilgard@utdallas.edu).

Kilgard, Michael P., Pritesh K. Pandya, Jessica Vazquez, Anil Gehi, Christoph E. Schreiner, and Michael M. Merzenich. Sensory input directs spatial and temporal plasticity in primary auditory cortex. J Neurophysiol 86: 326–338, 2001. The cortical representation of the sensory environment is continuously modified by experience. Changes in spatial (receptive field) and temporal response properties of cortical neurons underlie many forms of natural learning. The scale and direction of these changes appear to be determined by specific features of the behavioral tasks that evoke cortical plasticity. The neural mechanisms responsible for this differential plasticity remain unclear partly because important sensory and cognitive parameters differ among these tasks. In this report, we demonstrate that differential sensory experience directs differential plasticity using a single paradigm that eliminates the task-specific variables that have confounded direct comparison of previous studies. Electrical activation of the basal forebrain (BF) was used to gate cortical plasticity mechanisms. The auditory stimulus paired with BF stimulation was systematically varied to determine how several basic features of the sensory input direct plasticity in primary auditory cortex (A1) of adult rats. The distributed cortical response was reconstructed from a dense sampling of A1 neurons after 4 wk of BF-sound pairing. We have previously used this method to show that when a tone is paired with BF activation, the region of the cortical map responding to that tone frequency is specifically expanded. In this report, we demonstrate that receptive-field size is determined by features of the stimulus paired with BF activation. Specifically, receptive fields were narrowed or broadened as a systematic function of both carrier-frequency variability and the temporal modulation rate of paired acoustic stimuli. For example, the mean bandwidth of A1 neurons was increased (+60%) after pairing BF stimulation with a rapid train of tones and decreased (−25%) after pairing unmodulated tones of different frequencies. These effects are consistent with previous reports of receptive-field plasticity evoked by natural learning. The maximum cortical following rate and minimum response latency were also modified as a function of stimulus modulation rate and carrier-frequency variability. The cortical response to a rapid train of tones was nearly doubled if BF stimulation was paired with rapid trains of random carrier frequency, while no following rate plasticity was observed if a single carrier frequency was used. Finally, we observed significant increases in response strength and total area of functionally defined A1 following BF activation paired with certain classes of stimuli and not others. These results indicate that the degree and direction of cortical plasticity of temporal and receptive-field selectivity are specified by the structure and schedule of inputs that co-occur with basal forebrain activation and suggest that the rules of cortical plasticity do not operate on each elemental stimulus feature independently of others.

Although several studies have explored how parameters such as attention and task difficulty affect plasticity (Ahissar and Hochstein 1997; Ahissar et al. 1992; Edeline and Weinberger 1993; Recanzone et al. 1992c, 1993), relatively little is known about how specific features of behaviorally important stimuli direct cortical reorganization. In this study, we employ a powerful technique that mimics learning-induced plasticity to document how simple alterations of the sensory input produce substantially different forms of cortical plasticity (Juliano 1998; Kilgard and Merzenich 1998a,b).

Activity of cholinergic neurons in the basal forebrain (BF) provides a gate on plasticity mechanisms that allows the cortex to operate specifically on behaviorally arousing stimuli (Haselmo 1995; Singer 1986; Weinberger 1993; Woody 1982). Nucleus Basalis (NB) neurons provide the major source of cholinergic input to the neocortical mantle (Mesulam et al. 1983) (Fig. 1A) and contribute a significant GABAAergic input as well (Gritti et al. 1997). These neurons project ipsilaterally to all of the neocortex, as well as to the amygdala and the reticular nucleus of the thalamus (Levey et al. 1987; Mesulam et al. 1983), and receive inputs from the amygdala, ventral tegmentum, frontal cortex, hypothalamus, and from a number of brain stem nuclei (Haring and Wang 1986). NB neurons respond to both aversive and rewarding stimuli of different modalities and can be conditioned to respond to innocuous stimuli that become associated with reward (Pirch 1993; Richardson and DeLong 1991; Whalen et al. 1994).

Lesion studies support the hypothesis that NB activity serves as a reinforcement signal to guide cortical plasticity. Even the robust cortical reorganization that follows digit amputation, nerve section, or monocular deprivation can be blocked by NB lesions (Bear and Singer 1986; Juliano et al. 1991; Webster et al. 1991a). Highly selective lesions of only the cholinergic neurons in the NB prevent the plasticity that results from whisker trimming or follicle removal (Baskerville et al. 1997; Sachdev et al. 1998; Zhu and Waite 1998), providing strong evidence that NB is necessary for cortical map reorganizations.

The role of NB activity in gating cortical plasticity was further supported by experiments in auditory and somatosensory cortex of rats, guinea pigs, cats, and raccoons, demonstrating that pairing electrical activation of NB with sensory stimuli is sufficient to shift cortical receptive fields (Bakin and Weinberger 1996; Bjordahl et al. 1998; Edeline et al. 1994a,b; Hars et al. 1993; Howard and Simons 1994; Kilgard and Merzenich 1998a; Tremblay et al. 1990; Webster et al. 1991b), and temporal response properties (Kilgard and Merzenich 1998b; Shulz et al. 2000). Many of these experiments showed that NB-induced plasticity is blocked by atropine, a cholinergic antagonist. Introducing a 1-s separation between the sensory input and NB activation also blocked NB-induced plasticity (Metherate and Ashe 1991, 1993). Collectively, these results indicate that NB activity serves as a powerful modulator of cortical plasticity mechanisms.

Although cortical plasticity results from a medley of manipulations of sensory experience, it has generally been difficult to directly compare the results from such studies. In this study, the modality, species, behavioral state, and number of repet-
tions are the same across experimental groups that vary only in acoustic experience. The sound stimulus paired with BF activation was varied along a number of stimulus continua in different animals to explore how the structure and schedule of auditory input guides plasticity of spectral and temporal response properties. We also explored the effect of introducing a delay between tone onset and BF activation. Our results are consistent with previous studies of experience-dependent cortical plasticity in primates and document in greater detail how spectral and temporal features of the sensory input specify the direction and magnitude of receptive field and temporal response plasticity in primary auditory cortex (A1).

**METHODS**

**Implantation and stimulation**

BF-stimulating electrodes were implanted in 38 pentobarbital anesthetized (50 mg/kg) rats (~300 g). Platinum bipolar-stimulating electrodes (SNE-200, Rhodes Medical Instruments, Woodland Hills, CA) were lowered 7.0 mm below the cortical surface 3.3 mm lateral and 2.3 mm posterior to bregma and cemented into place using sterile techniques approved under University of California at San Francisco and University of Texas at Dallas animal care protocols. Rats received prophylactic treatment with ceftriaxone antibiotic (20 mg/kg), dexamethasone (4 mg/kg), and atropine (1 mg/kg). Three bone screws were used to anchor the electrode assembly. Leads were attached to screws over the cerebellum and cortex so that the global electroencephalograph (EEG) could be monitored during BF activation in unanesthetized animals.

After 2 wk of recovery, ionic stimuli were paired with BF electrical stimulation in a sound-shielded test chamber (5 days/wk) for 1 mo (Table 1). Animals were placed in a 25 × 25-cm wire cage in the middle of 60 × 70-cm box lined with 3-in acoustic foam. The cage was positioned 20 cm below the audio speaker. A small 4-pin connector attached to a swivel was used to record the EEG and to deliver short current pulses to the stimulating electrode. Each animal received 300–500 pairings of tones and BF stimulation per day. Interstimulus intervals varied randomly from 10 to 30 s. Ten rats received BF stimulation paired with a 70 dB SPL tone with a fixed frequency (4, 1 kHz). In five rats, nine different randomly interleaved tone frequencies were paired with BF stimulation (4 and 19 kHz). In five rats, nine different randomly interleaved tone frequencies were paired with BF stimulation (1.3, 2, 3, 4, 5, 7, 9, 11, and 14 kHz). In this group, tones were presented at 30–40 dB above rat hearing threshold (Kelly and Masterton 1977) to activate similarly sized neural populations. In four rats, a train of six short 9-kHz tones presented at 15 pulses per second (pps) were paired with BF stimulation. In 10 rats, trains of short tones applied at a constant tone frequency which varied randomly from trial to trial (1.3, 2, 3, 5, 9, 14, or 19 kHz at 20–30 dB above threshold). The repetition rate of the tones was fixed for each animal (5, 7.5, and 15 pps, n = 4, 2, and 4 rats, respectively). All tones had 3-ms onset and offset ramps. The tones paired with BF stimulation were 250 ms in duration except for the tone trains that were composed of 25-ms tones.

To establish the specificity of BF pairing, several animals were also stimulated with tones that were not paired with BF stimulation. Half of the animals in the single-frequency group were also presented, on the same schedule, with two other tone frequencies not paired with BF stimulation (see Table 1). There were no unpaired stimuli delivered to the 9 kHz/15-pps rats. The multiple-frequency train groups heard one of the multiple of the multiple-frequencies tone pips presented in isolation without BF stimulation as often as they heard each train that was paired with BF stimulation.

When a single unmodulated tone was used as the auditory stimulus (one frequency group), electrical stimulation began 50 ms after tone onset in half the experiments and 200 ms before tone onset in the other half (Fig. 1B). Although some forms of learning are very sensitive to the order of sensory and modulatory inputs, these two relative timings did not generate noticeably different plasticity effects, and the two groups are analyzed together in this study. In the multiple-carrier frequency groups, electrical stimulation began 50 ms after tone onset. When tone trains were used, stimulation occurred simultaneously with the onset of the fourth tone in trains. In four animals, 19-kHz tones were presented 10 s after each BF stimulation. BF stimulation consisted of 20 capacitatively coupled biphasic pulses (0.1-ms pulse width, 100 pulses/s).

The efficacy of BF activation was continuously monitored in every animal by quantifying BF-induced EEG desynchronization during slow-wave sleep. The current level (70–150 μA) for BF stimulation was chosen for each animal to be the minimum necessary to desynchronize the EEG for 1–2 s during slow-wave sleep. After observing many naturally occurring sleep-wake cycles in each animal using video monitoring, we determined a level of EEG power (from 1 to 5 Hz) that distinguished the two states (i.e., always below while awake

<table>
<thead>
<tr>
<th>Experiment Group</th>
<th>Parameters Varied</th>
<th>Auditory Stimuli Paired With BF Stimulation</th>
<th>Unpaired Stimuli</th>
<th>No. of Rats</th>
<th>No. of A1 Sites</th>
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<tbody>
<tr>
<td>Control</td>
<td>Ø</td>
<td>Ø</td>
<td>Ø</td>
<td>14</td>
<td>663</td>
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<tr>
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<td></td>
<td></td>
<td>9 kHz</td>
<td>[4 and 19 kHz]</td>
<td>4</td>
<td>233</td>
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<tr>
<td></td>
<td></td>
<td>19 kHz</td>
<td>[4 and 19 kHz]</td>
<td>2</td>
<td>112</td>
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<tr>
<td>Multiple-carrier frequencies</td>
<td>Number of paired frequencies</td>
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<td>9 and 19 kHz</td>
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<tr>
<td>15 pps 9 kHz</td>
<td>Repetition rate and number of frequencies</td>
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<td>5</td>
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</tr>
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<td>15 pps train of tones, 9 kHz</td>
<td>Ø</td>
<td>4</td>
<td>224</td>
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<tr>
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<td></td>
<td>15 pps train of tones, multiple frequencies</td>
<td>Single tones of multiple frequencies</td>
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<td>223</td>
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<tr>
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<td>Single tones of multiple frequencies</td>
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<td>92</td>
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<tr>
<td>5 pps multi</td>
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<td>5 pps train of tones, multiple frequencies</td>
<td>Single tones of multiple frequencies</td>
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<td>Delayed BF</td>
<td>Relative timing</td>
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<td>Totals</td>
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<td></td>
<td></td>
<td>52</td>
<td>2616</td>
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Basal forebrain (BF) stimulation was paired with 10 classes of auditory stimuli. Four features of the paired auditory stimuli (tone frequency, number of tone frequencies, repetition rate, and onsets timing) were varied to determine their effect on cortical plasticity. Brackets denote stimuli that were played in half of the one frequency experiments to determine the effect of unpaired stimuli.

**Table 1. Summary of experiments**

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Parylene-coated tungsten microelectrodes (FHC, 250–1,000 μA) for BF stimulation to be the minimum level that desynchronized the EEG below the EEG threshold. Typically, rats were sleeping during 10–20% of stimulation events, and BF activation resulted in desynchronization for 75–95% of these events. Only trials with low-frequency EEG power above the threshold before stimulation were analyzed to determine effectiveness of BF activation. EEG desynchronization usually lasted 1–4 s. Tonal and electrical stimuli did not evoke any observable behavioral responses (i.e., did not cause rats to stop grooming, or awaken, if sleeping).

Electrophysiological recordings and analysis

This study is based on neuronal spike data collected from 2,616 microelectrode penetrations into the right primary auditory cortex in 52 adult female Sprague-Dawley rats. Surgical anesthesia was induced with pentobarbital sodium (50 mg/kg). Throughout the surgical procedures and during the recording session, a state of areflexia was maintained with supplemental doses of dilute pentobarbital (8 mg/ml ip). The trachea was cannulated to ensure adequate ventilation and to minimize breathing-related noises. The skull was supported in a head holder that left the ears unobstructed. The cisternae magna was drained of CSF to minimize cerebral edema. After reflecting the temporalis muscle, auditory cortex was exposed and the dura was resected. The cortex was maintained under a thin layer of viscous silicon oil to prevent desiccation. The location of each penetration was reproduced on a ×40 digitized image of the cortical surface microvasculature.

The primary auditory cortex was defined on the basis of its short-latency (8–20 ms) responses and its continuous tonotopy (preferred tone frequency increased from posterior to anterior, see Fig. 2, A and B) (Kilgard and Merzenich 1999). Responsive sites that exhibited clearly discontinuous best frequencies and long-latency responses, unusually high thresholds, or very broad tuning were considered to be non-A1 sites. Penetration sites were chosen to avoid damaging blood vessels while generating a detailed and evenly spaced map. Voronoi tessellation (Matlab 5.2, MathWorks) was used to visualize the topography of A1. Voronoi tessellation generates polygons from each set of nonuniformly spaced recording sites such that every point within each polygon was nearer to the sampled site for that polygon than to any other site. The boundaries of the map were functionally determined using nonresponsive and non-A1 sites.

Recordings were made in a shielded, double-walled sound chamber (IAC). Action potentials were recorded simultaneously from two Parylene-coated tungsten microelectrodes (FHC, 250–μm separation, 2 MΩ at 1 kHz) that were lowered orthogonally into the cortex to a depth of 550 μm (layers IV/V). The neural signal was filtered (0.3–8 kHz) and amplified (10,000×). Action potential waveforms were recorded whenever a set threshold was exceeded, allowing off-line spike sorting using Autocut (Datawave) or Brainware (Tucker-Davis Technology) software. Although most responses in this study represented the spike activity of several neurons, single units were separated when possible, confirming that single units exhibited tuning that was qualitatively similar to multi-unit response samples. To minimize experimenter-induced sampling bias the experimenter was blind to the frequency(ies) paired with BF stimulation.

In most experiments, acoustic stimuli were delivered to the left ear via a calibrated ear phone (STAX 54) positioned just inside the pinnae. In the experiments with nine carrier frequencies, stimuli were experienced blind observer using custom software that displayed raw spike data without reference to the frequencies and intensities that generated the responses. For each tuning curve, best frequency, threshold, bandwidth (10, 20, 30, and 40 dB above threshold), and latency data were recorded (Fig. 1C). Characteristic frequency (CF) is the frequency that evokes a consistent neural response at the lowest frequency response tuning curves were determined by presenting 45 frequencies spanning 3–4.5 octaves centered on the approximate best frequency of the site, or 81 frequencies from 1 to 32 kHz. Each frequency was presented at 15 or 16 intensities ranging between 0 and 75 dB (either 675 or 1,296 total stimuli). Tuning curve tones were randomly interleaved and separated by 500 ms. All tonal stimuli used during the acute phase of this study were 25-ms long, including 3-ms rise and fall times.

Rat A1 tuning curves were V-shaped and generally exhibited monotonic intensity response functions (Kilgard and Merzenich 1999; Sally and Kelly 1988). Tuning-curve parameters were defined by an experienced blind observer using custom software that displayed raw spike data without reference to the frequencies and intensities that generated the responses. For each tuning curve, best frequency, threshold, bandwidth (10, 20, 30, and 40 dB above threshold), and latency data were recorded (Fig. 1C). Characteristic frequency (CF) is the frequency that evokes a consistent neural response at the lowest frequency response tuning curves were determined by presenting 45 frequencies spanning 3–4.5 octaves centered on the approximate best frequency of the site, or 81 frequencies from 1 to 32 kHz. Each frequency was presented at 15 or 16 intensities ranging between 0 and 75 dB (either 675 or 1,296 total stimuli). Tuning curve tones were randomly interleaved and separated by 500 ms. All tonal stimuli used during the acute phase of this study were 25-ms long, including 3-ms rise and fall times.

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to experimentally naïve controls (663 A1 penetrations) and discussed in relation to several mechanisms that direct these opposite forms of plasticity remain unclear. In our experiments, varying the carrier frequency of tones trains with random carrier frequency and 5- or 7.5-pps repetition rate as part of our experiments on temporal plasticity (Kilgard and Merzenich 1998b). The systematic decrease in receptive-field size, while discriminating between different tone frequencies decreases receptive-field size (Recanzone et al. 1992c, 1993). Although it was argued that the differential plasticity effects observed in those studies contributed to the practice-induced improvements in task performance, the mechanisms that direct these opposite forms of plasticity remain unclear. In our experiments, varying the carrier frequency of the 15-pps tone trains resulted in significantly less receptive-field expansion ($P < 0.0001$) compared with 15-pps trains with a fixed carrier frequency (Fig. 3, a and b). We also presented tone trains with random carrier frequency and 5- or 7.5-pps repetition rate as part of our experiments on temporal plasticity (Kilgard and Merzenich 1998b). The systematic decrease in receptive field expansion as repetition rate is decreased (Fig. 3, a–d) suggests that cortical plasticity rules shape receptive field size dependent on input repetition rate.

We also observed that unpaired (background) stimuli could
influence receptive-field plasticity. Although receptive-field sizes were increased by 20% when a single tone was paired with BF activation, frequency selectivity was not affected in a different group of rats that received identical BF pairing with one tone frequency but also heard two additional frequencies that were not paired with BF stimulation (Fig. 3, e–g). This result supports the preceding interpretation that frequency variability tends to minimize receptive field expansion and also reveals an important role of background sounds in shaping cortical plasticity.

**Strength of evoked response**

The strength of the evoked response of A1 neurons could also be increased by BF-induced plasticity mechanisms. Of the 10 different sets of acoustic stimulation paired with BF activation, only 1 significantly altered the mean number of spikes evoked per tone. After pairing the 15-pps trains of 9-kHz tones, on average 3.7 ± 0.2 spikes per tone were recorded from each A1 penetration compared with 2.8 ± 0.1 spikes in experi-

tally naïve rats. This increased excitability was likely caused by the dramatic overlap of receptive fields due to the combination of map reorganization and receptive field broadening. Pairing multiple carrier frequencies with a slow repetition rate (in isolation, 5 or 7 pps) decreased the spontaneous firing rate (by ~30%; \( P < 0.05 \)) compared with controls.

Previous studies using cholinergic modulation observed highly specific changes in the number of spikes evoked by different tones within a neuron’s receptive field. In some cases, the neural response to frequencies within one-fourth of an octave were facilitated, while the responses to other nearby frequencies were inhibited (Bakin and Weinberger 1996; McKenna et al. 1989; Metherate and Weinberger 1989, 1990). Most of the analysis in this study is focused on the receptive field as a unit and would not pick up changes in the response strength to frequencies within the tuning curve. To determine if such precise effects resulted from our long-term pairing of BF activation with tonal stimuli, the number of spikes evoked as a function of frequency was also examined for every tuning curve. We observed no consistent peak at the paired frequency in individual sites or in the population as a whole (data not shown). Minimum stimulus thresholds also showed no consistent change as a result of pairing BF stimulation with any of the auditory stimuli used in this study.

**Temporal response plasticity**

Aspects of the sensory input had a significant effect on the latency of A1 responses to tones (Fig. 4). Pairing a slow train of tones with multiple carrier frequencies increased the average minimum response latency by ~1 ms, while pairing a single tone with BF stimulation (1 at a time or in 15-pps trains) decreased onset latencies by ~1 ms. Both of these sets of acoustic stimuli delayed the end of the cortical response (Fig. 4B). The widening of the evoked response after single tone pairing likely reflects the consequences of the expanded cortical map in these animals. In contrast, the increase in latency when the maximum repetition rate is decreased (Kilgard and Merzenich 1998b) supports earlier observations that minimum latency is correlated with maximum following rate (Schreiner et al. 1997). Pairing nine different tones with BF stimulation generated a distinct form of temporal plasticity. The population discharge (response synchrony) was significantly sharpened by an increased onset latency combined with a decreased duration of the cortical response. This result suggests that the statistics of the sensory input determine whether spectral or temporal strategies are used to sharpen the cortical representation of stimuli paired with BF activation. This interpretation is strengthened by our observation that pairing two different tones (intermediate between one and nine tone pairing) caused no change in response latency. Thus our results indicate that the temporal response properties of cortical neurons can be substantially and systematically altered by spatial and temporal features of the sensory environment.

We have previously reported that the maximum repetition rate that A1 neurons can respond to can be increased or decreased depending on the rate of acoustic stimuli paired with BF activation (Kilgard and Merzenich 1998b). Additional experiments indicate that repetition rate is not the only stimulus feature that guides the expression of temporal selectivity. Spectral variability also influenced whether maximum following
rate was altered. We paired 15-pps tone trains with BF activation in two groups of animals and quantified the resulting plasticity in following rate by deriving RRTFs at every site. The maximum following rate of cortical neurons was not altered by pairing BF stimulation with 15-pps, 9-kHz trains (Fig. 5). The profound map reorganization that resulted indicates that the mechanisms of cortical plasticity were successfully engaged (Fig. 6A). In a different set of rats, random carrier frequency 15-pps tone trains were paired with BF activation to test whether temporal plasticity had been prevented by the extent of map reorganization or whether the 9-kHz carrier frequency had simply been a more salient feature than the repetition rate of 15 pps. Varying the carrier frequency caused the mechanisms of cortical plasticity to significantly increase the cortical following rate (Fig. 5). Although this variation prevented the map reorganization that occurs when a fixed carrier is used (Fig. 6B), it is not clear whether preventing map expansion or increasing the relative saliency of the temporal modulation is a more accurate explanation. Either way this result demonstrates that spectral and temporal characteristics of sounds interact to control spectrotemporal selectivity in cortical neurons. Thus it may be difficult to predict cortical plasticity in response to complex stimuli (i.e., vocalizations) from studies of synaptic mechanisms or cortical plasticity evoked by elemental stimuli.

Expansion of functionally defined A1

In addition to increasing the percent of A1 that responded to the paired tone frequency (Kilgard and Merzenich 1998a), pairing BF activation with a single frequency increased the total area of A1 by 50% (Fig. 7). Although this increase in A1 area was based on the well-established functional definition that the primary auditory field has phasic, short-latency responses to tones and a continuous tonotopy (Kilgard and Merzenich 1999; Sally and Kelly 1988), we do not know the effect on anatomical definitions of primary auditory cortex (Roger and Arnault 1989; Romanski and LeDoux 1993). The observation that the size of A1 was not significantly increased by any of the other stimulus sets paired with BF activation indicates that this form of cortical plasticity is specific to certain forms of acoustic experience (Fig. 7). When the CF shift and overall expansion of A1 are considered together, pairing a single tone with BF stimulation was able to increase the number of A1 neurons responding to the paired tone by threefold.

Frequency map plasticity

Although map reorganizations occur in some forms of natural learning (Xerri et al. 1994, 1996), such reorganizations typically result from sensory input that is restricted to one region of the topographic map. Learning still occurs in many situations where the distribution of stimuli along the receptor surface precludes map expansion as a possible mechanism. As expected, we observed no significant map plasticity in any of the five rats that heard nine different randomly interleaved unmodulated tones paired with BF activation (data not shown). The increased frequency selectivity and improved temporal synchronization of the cortical response described in the preceding text supports the hypothesis that both receptive field and temporal plasticity contribute to behavioral improvements when it is not possible to increase the number of engaged neurons via map reorganization.

To test the importance of the temporal relationship between BF activation and sensory input, we delivered BF activation with a 10-s interval before 19-kHz tone presentation. Earlier studies showed that a 1-s separation between sensory input and BF activation caused no short-term BF-induced plasticity (Metherate and Ashe 1991, 1993). In our chronic preparation, a 10-s separation resulted in a general decrease in frequency tuning (BW10 was 120 ± 4% of controls, \( P < 0.001 \)) but did not result in a specific map expansion at the paired frequency (data not shown).
DISCUSSION

Experimental manipulations of sensory experience can result in a variety of changes in cortical responsiveness (Byrne and Calford 1991; Hubel and Wiesel 1970). As a class, such effects are generally called experience-dependent plasticity. Merzenich and colleagues observed that different forms of cortical plasticity developed during extended operant training of owl monkeys on several different tasks (Jenkins et al. 1990; Recanzone et al. 1992a, c). Although expansion and sharpening of cortical representations of behaviorally relevant stimuli was a common theme among these studies, the mechanisms that allow the cortex to adapt its processing of sensory information to improve behavioral performance remain unclear. It has been hypothesized that much of the information the cortex uses to determine how to reorganize itself is contained in the sensory input and may even be relatively independent of specific task goals (Ahissar and Ahissar 1994; Merzenich et al. 1990).

This study represents our initial efforts to systematically vary the sensory input to elucidate the “rules” that allow sensory experience to shape both spectral and temporal responses of cortical neurons in adult animals. We used electrical stimulation of BF to activate cortical plasticity mechanisms and varied only the paired sensory stimuli to explore the relationship between the statistics of the sensory input and the class, direction, and magnitude of cortical reorganization. We report that stimulus repetition rate and spectral variability systematically alter a number of cortical response parameters, including characteristic frequency, frequency bandwidth, size of A1, cortical excitability, stimulus following rate, and response latency (Table 2). The observation that systematic changes in sensory input result in systematic changes in cortical information processing supports the hypothesis that simple rules govern experience-dependent cortical plasticity.

BF-induced spectral and temporal reorganizations

Our results clarify how specific aspects of the sensory input influences neural selectivity. The receptive-field plasticity recorded in this study provides strong evidence that rules exist in the cortex to translate sensory input into substantive changes in cortical information processing. Frequency bandwidth was particularly sensitive to the auditory stimulus paired with BF activation. Bandwidth was increased by 60% or decreased by 25% simply by pairing different tonal stimuli with identical BF stimulation. Across the range of stimulus classes used in this study, bandwidth increased systematically with increasing rep-
petition rate and decreased with increasing spectral variability (Fig. 8A).

Merzenich and colleagues observed a similar relationship following operant training of monkeys. Cortical receptive-field size was decreased by practicing tasks with stimuli delivered to different locations on the receptor surface (cochlea or skin) and were increased by training on a task requiring detection of changes in the modulation rate of a stimulus delivered to an invariant skin location (Jenkins et al. 1990; Recanzone et al. 1992a,c). The authors suggest that the observed training-induced changes in receptive-field size were consistent with the operation of Hebb-like synapses driven to change by temporally coherent inputs in a competitive cortical network. Specifically, they postulated that larger receptive fields are generated by the temporally synchronous activity in response to low-frequency (10–20 Hz) stimulation at an invariant location of the receptor surface, while decreased receptive fields resulted from asynchronous cortical activity in response to stimuli that move across or are applied at inconsistent receptor locations (skin or cochlea). By systematically varying both spectral variability and repetition rate, our study strengthens the argument that receptive-field size is determined by the structure of temporal correlations evoked by input sources and supports the hypothesis that simple rules operate in the cortex to generate useful changes in circuitry based on the statistics of sensory stimuli marked by BF activity.

Our results also support earlier findings that receptive-field plasticity effects are not always limited to the region of the map most strongly activated by the training stimulus. Expansion of somatosensory receptive fields following vibrotactile training using one digit was observed on neighboring digits as well the trained digit (Recanzone et al. 1992c). Statistical analysis of receptive-field size in rats that heard one frequency paired with BF stimulation revealed that expansion also occurred in neurons with CFs up to two octaves away from the paired frequency (data not shown).

BF stimulation has been shown to increase the number of stimulus-evoked spikes (Bakin and Weinberger 1996; Edeline et al. 1994a,b; Tremblay et al. 1990; Webster et al. 1991b). Of the seven classes of stimuli paired with BF stimulation in this study, only 15-pps trains of 9-kHz tones caused a significant increase in evoked response strength (spikes/tone). Recanzone and colleagues also observed an increase in evoked responses after training monkeys on a task that involved the analogous tactile stimulus (a 20-Hz vibration of a single-digit segment). Thus our findings are consistent with previous demonstrations that response strength plasticity is dependent on particular features of sensory inputs.

Electrical activation of the BF paired with tonal stimuli was sufficient to generate significant reorganization of the A1 frequency map (Kilgard and Merzenich 1998a). The map reorganization combined with a generalized expansion of A1 to generate a threefold increase in the number of cortical neurons

<table>
<thead>
<tr>
<th>TABLE 2.</th>
<th>Schematic summary of experimental results</th>
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<tr>
<td>One frequency</td>
<td>↑↑</td>
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<tr>
<td>Two frequencies</td>
<td>↑</td>
</tr>
<tr>
<td>Nine frequencies</td>
<td>0</td>
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<tr>
<td>15-pps tone trains</td>
<td>∥∥</td>
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<tr>
<td>One-carrier frequency</td>
<td>0</td>
</tr>
<tr>
<td>Seven-carrier frequencies</td>
<td>0</td>
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<td>5-pps tone trains</td>
<td>0</td>
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Both the degree and direction of cortical plasticity [including changes in receptive field structure, primary auditory cortex (A1) area, response strength, temporal selectivity, and response latency] are influenced by the structure and schedule of inputs that co-occur with nucleus basalis activity. The direction and number of arrows indicate direction and magnitude of observed plasticity. Zeros indicate no significant difference from naive controls. Dash indicates not evaluated.
that responded to the paired frequency. The direction of tuning curve shift was determined by the frequency of the tones paired with BF stimulation, while the magnitude of map expansion was determined by the degree of spectral variability of the paired tones. Our results support earlier reports that BF activity generates the most precise cortical plasticity when nearly simultaneous with cortical input (Metherate and Ashe 1991, 1993). This study extends previous reports that the absolute size of a cortical zone could be expanded following some types of behavioral training, if attentional resources were appropriately engaged (Jenkins et al. 1990; Merzenich et al. 1990). We conclude that BF activity is sufficient to mimic these cortical map expansions.

The maximum following rates of A1 neurons were decreased or increased by pairing BF stimulation with 5- or 15-pps tone trains, respectively (Kilgard and Merzenich 1998b). This report extends those findings by demonstrating that the degree of spectral variability can substantially alter the expression of temporal plasticity in auditory cortex. Pairing a train of 9-kHz tones presented at 15 pps with BF stimulation did not increase the maximum cortical following rate (Fig. 5). This result may explain why the cortical recovery time was not altered by many weeks of training monkeys on a temporally based tactile discrimination task that used spatially restricted input (Recanzone et al. 1992d). In that study, Recanzone and colleagues argued that decreased latency and increased synchronization contributed to improved behavioral performance.

Finally, our finding that response latency is systematically altered by certain classes of acoustic stimuli provides another potential explanation for an earlier plasticity result using monkeys (Fig. 8B). Recanzone and colleagues observed that training monkeys to distinguish a tone standard from a range of other tone frequencies caused minimum latency to increase (Recanzone et al. 1993). As in that study, latency was increased in our study when a range of frequencies was presented (Fig. 8B). However, this increase in minimum latency was accompanied by a decrease in the duration of the cortical response that generated a more synchronous evoked response (and a decrease in spontaneous activity). If the duration of the cortical response in the earlier study (not reported) was decreased, an apparent distinction between the two monkey studies may point to a commonality that more synchronous activation of cortical neurons results from extensive discriminative training. The development of receptive field and temporal refinement when stimuli are distributed across the receptor surface suggests that these mechanisms may support behavioral improvements when map expansion is not possible.

Potential mechanisms that underlie the cortical plasticity documented in this study include changes in network, synaptic, or cell intrinsic properties. Although it is likely that effects at all three levels contributed to the observed changes in spatial and temporal response properties, the simplest explanation of our results is that sensory experience differentially affected the balance of inhibition and excitation. Blocking GABAergic receptors in the auditory cortex results in receptive field expansion, increased response strength, and decreased latency (Chen and Jen 2000; Wang et al. 2000). In our experiments, pairing a 15-pps train of 9-kHz tones with BF activation caused very similar effects (Fig. 8A and B, top right). Opposite changes in all three response characteristics occurred when unmodulated tones of varying carrier frequency were paired (Fig. 8, A and B, bottom left). Recent computational models with spike-timing-dependent synaptic plasticity have shown that such selective mechanisms can also profoundly affect response latency (Song et al. 2000). Although additional experiments are needed to clarify the mechanisms that underlie these changes, the systematic relationship between sensory experience and cortical plasticity documented in this study suggests that a comprehensive description of the rules that transform experience into useful changes in the distributed cortical response is possible.

Although several studies have reported that the cortical plasticity induced by a single episode of BF stimulation decays rapidly, other studies have observed longer-lasting effects (Bjordahl et al. 1998; Dykes et al. 1990; Edeline et al. 1994a; Hars et al. 1993; Rasmusson and Dykes 1988; Tremblay et al. 1990; Webster et al. 1991b). ShulZ and colleagues recently
demonstrated that in some situations acetylcholine-dependent plasticity is expressed only in the presence of acetylcholine (Shulz et al. 2000). Both the speed of acquisition and volatility of these effects supports their argument that state-dependent levels of neuromodulators control the expression of some forms of cortical plasticity. All of the data presented in this study was collected 24–48 h after the last electrical activation of BF. Our observation that BF-induced plasticity endures for 1 day and is expressed even under anesthesia suggests that structural changes may contribute to the expression and maintenance of the changes in neural selectivity documented in this study. Thus the duration and size of the plasticity effects generated by repeated BF activation suggest that short-lived BF-induced plasticity can become long-lasting with extended repetition over the course of days to weeks.

Technical considerations

Although several other studies using BF stimulation have demonstrated that activation of cholinergic receptors is necessary for BF-induced plasticity (Bakin and Weinberger 1996; Edeline et al. 1994b; Hars et al. 1993; Kilgard and Merzenich 1998a; Metherate and Ashe 1991), the role of acetylcholine has not been established in this study. Although we suspect acetylcholine is involved in the plasticity documented in this report, it is also likely that other neurotransmitters released by NB neurons (including GABA) are important regulators as well (Dykes 1997; Gritti et al. 1997). The aim of this study was to clarify how different sounds paired with BF activation lead to different forms of cortical plasticity.

Two types of comparisons were used to quantify the effect of acoustic experience paired with BF activation. In the first, cortical responses from experimentally naïve rats were compared with responses from rats that had received 4 wk of BF stimulation. This across-animal design was necessary due to the difficulty with generating a detailed reconstruction of the cortical map before and after pairing in individual animals. Rats were randomly selected to serve as control or experimental animals. Thus the responses of A1 neurons in naïve animals should be equivalent to responses in experimental animals prior to BF stimulation, and significant differences with this group reflect experimentally induced plasticity. The second class of comparisons were between groups of rats that had received identical BF stimulation and differed only in their acoustic experience. These comparisons establish the specificity of the plasticity effects documented in this study and rule out the possibility that the observed changes in cortical responses arose due to BF implantation or other nonspecific effects.

Although BF activation occurred only in unanesthetized animals, the neural responses analyzed in this study were collected under barbiturate anesthesia. Cortical responses are unlikely to be identical in awake and anesthetized animals; however, basic response features of barbiturate anesthetized cortex, such as frequency tuning and repetition rate transfer functions, are at least qualitatively similar to the awake state (deCharms et al. 1998; Hars et al. 1993; Recanzone et al. 2000; Shamma and Symmes 1985). In this study, all of the comparisons of neural responses were between rats anesthetized in a similar manner. Thus anesthesia is unlikely to be responsible for the differential plasticity documented here.


correlation with the hypothesis that an important function of this activity is to mark individual events as behaviorally relevant so that cortical plasticity mechanisms can improve the representations of important stimuli (Ahissar and Ahissar 1994; Richardson and DeLong 1991; Singer 1986; Weinberger 1993). Although essential for effective learning, identifying behaviorally important stimuli represents only an initial step toward generating an improved cortical representation that might be behaviorally useful. Individual neurons must not only alter their response properties based only on their synaptic inputs; they must do so in a concerted manner that leads to an improved distributed response.

Although it seems obvious that the representation of a tone would be improved by increasing the number of neurons tuned for the tone’s frequency, in fact, the ideal solution depends entirely on what information is needed from the stimulus. If an animal is conditioned that a tonal stimulus predicts footshock, there is no way to know which features of the stimulus will predict shock in the future (frequency, duration, rise time, bandwidth, intensity, modulation rate, etc.). The fact that animals generalize indicates that they do not assume that all of the features are required. Evolution may have shaped brain circuitry to make default guesses that are appropriate based on the evolutionary history of the species (i.e., phyletic memory) (see Fuster 1995). These guesses may take the form of rules that operate within the brain to extract stimulus features that are most likely to contain relevant information.

A substantial amount of literature now demonstrates that different behavioral tasks result in different forms of representational plasticity in the cortex. Although the relationship between stimulus representation and information processing is far from clear, the similarity between the results in this study and earlier reports of cortical plasticity evoked by extended behavioral training suggests that the sensory input itself can provide much of the information about how to improve sensory representations. In this initial study we have focused on two stimulus features, repetition rate and spectral variability, and observed that each affected cortical plasticity in a systematic manner (Fig. 8). These results indicate that the cortex uses these features to guide several forms of cortical plasticity, including reorganization of feature maps, plasticity of spectral and temporal selectivity, expansion of a primary sensory cortical field, and increased strength of evoked responses. Additional experiments are needed to determine how other stimulus parameters shape representational plasticity.

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REFERENCES


