Amplitude and Frequency Dependence of Spike Timing: Implications for Dynamic Regulation

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**Running head:** Amplitude dependent resonance for reliability

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The spike time reliability of motoneurons in the Aplysia buccal motor ganglion was studied as a function of the frequency content and the relative amplitude of the fluctuations in the neuronal input, calculated as the coefficient of variation (CV). Measurements of spike time reliability to sinusoidal and aperiodic inputs, as well as simulations of a noisy leaky integrate-and-fire neuron stimulated by spike trains drawn from a periodically modulated process, demonstrate that there are three qualitatively different CV-dependent mechanisms that determine reliability: 1) noise-dominated (CV<0.05 for Aplysia motoneurons) where spike timing is unreliable regardless of frequency content; 2) resonance-dominated (CV ≈ 0.05-0.25) where reliability is reduced by removal of input frequencies equal to motoneuron firing rate; and 3) amplitude-dominated (CV>0.35) where reliability depends on input frequencies greater than motoneuron firing rate. In the resonance-dominated regime, changes in the activity of the presynaptic inhibitory interneuron B4/5 alter motoneuron spike time reliability. The increases or decreases in reliability occur coincident with small changes in motoneuron spiking rate due to changes in interneuron activity. Injection of a hyperpolarizing current into the motoneuron reproduces the interneuron-induced changes in reliability. The rate-dependent changes in reliability can be understood from the phase locking properties of regularly spiking motoneurons to periodic inputs. Our observations demonstrate that the ability of a neuron to support a spike time code can be actively controlled by varying the properties of the neuron and its input.

Key words: spike time reliability, synchrony, central cholinergic synapses, Aplysia, integrate-and-fire model neuron
INTRODUCTION

Noise, variability and randomness are ubiquitous characteristics of the nervous system, yet under appropriate conditions, both vertebrate (Kröller et al., 1988; Mainen and Sejnowski, 1995; Berry et al., 1997; de Ruyter van Steveninck et al., 1997; Haas and White, 2002;) and invertebrate (Bryant and Segundo, 1976; Haag and Borst, 1997; Hunter et al., 1998) neurons can generate precisely timed action potentials. This paradox has attracted considerable attention to the mechanisms that determine the precision of a neuron's output.

The spike timing reliability of a single event is related to the slope of the membrane potential at threshold crossing: neurons fire reliably in the presence of noise if the input causes a steep increase in membrane potential at the time of threshold crossing (Stein, 1967; Goldberg et al., 1984; Gerstner et al., 1996; Hunter et al., 1998). However, this explanation does not account for reliability measured across an entire spike train. Consequently a number of investigations have focused on the interplay between the properties of the neuron and the statistical properties of its input. A variety of mechanisms become important. These include resonance between the input spectrum and neuronal spiking rate (Jensen, 1998; Hunter et al., 1998; Fellous et al., 2001; Haas and White, 2002), the presence of multiple stable attractors and their stability (Foss and Milton, 2000; Pakdaman, 2002; Tiesinga et al., 2002), and more complex membrane properties, such as the presence of subthreshold oscillations and persistent currents (Fellous et al., 2001; Haas and White, 2002; Shalinsky et al., 2002; Svirskis et al., 2002).

Two different interpretations concerning the relationship between the frequency content of the neuronal input and spike timing reliability have arisen: 1) increasing stimulus power, particularly in high frequency bands, increases reliability (Mainen and Sejnowski, 1995; Schneidman et al., 1998; Yamanobe and Pakdaman, 2002) and 2) increasing stimulus power in the frequency band corresponding to the intrinsic firing rate of the neuron increases reliability (Hunter et al., 1998; Jensen, 1998; Haas and White, 2002); for discussion see Haas and White (2002). That spike timing reliability can exhibit both types of dependencies has been underemphasized. The key point is that the mechanism for spike timing reliability depends on the relative amplitude of the fluctuations in the input, calculated as the coefficient of variation (CV) (Hunter et al., 1998; Jensen, 2002). We investigate this amplitude dependence for several types of inputs in the Aplysia buccal ganglion and the leaky integrate and fire model.

The importance of the resonance mechanism is the implication that spike timing reliability can be sensitively and rapidly controlled with only small changes in neuronal firing rate. To illustrate this concept, we use the inhibitory buccal interneuron B4/5 to alter motoneuron firing rate, either increasing or decreasing reliability, consistent with the resonance mechanism. Because the control of spike time reliability is closely related to control of synchrony in an uncoupled neuronal population receiving a coherent input (Knight, 1972, Collins, et al 1995), this provides a mechanism by which synaptic or neuromodulatory input can dynamically regulate synchrony with only small changes in population firing rate (Vaadia et al., 1995, Hopfield and Brody, 2001).

METHODS
Aplysia electrophysiology

*Aplysia* care and dissection were performed as described in Church and Lloyd (1994). The ganglion was constantly perfused with artificial seawater containing high divalent cations; perfusion solution concentrations in mM/L: 286NaCl, 165MgCl, 10KCl, 33CaCl, 5NaCOH. The high divalent solution raises the threshold for neural firing and serves to quiet intrinsic network firing while allowing for the investigation of specific synapses, presumably via the mechanism of Gouy-Chapman charge screening (Gardner, 1990; Hille, 1992).

Recordings of the postsynaptic neuron were made in two electrode current clamp mode using an AxoClamp 2B amplifier (Axon Instruments, Foster City, CA) with electrode resistances ≈4MΩ. The presynaptic interneuron B4/5 was identified based on size, location and the criterion that it generates inhibitory postsynaptic currents in buccal motoneurons. It was stimulated to fire action potentials with a constant current DC input and a sinusoidal input to regularize its firing using a second AxoClamp 2B amplifier in current clamp mode. B4/5 can mediate pure inhibitory, pure excitatory, or diphasic inhibitory/excitatory conductances depending on the follower cell; only pure inhibitory follower cells were investigated (identified as B3, 6, 8, or 9 in Gardner and Kandel, 1977).

Data were low pass filtered at 1kHz with a Frequency Devices 902 low pass filter (Frequency Devices, Haverhill, MA) and digitally sampled at 2kHz. All recording and stimulation protocols were automated using an AD2210 A/D board (Real Time Devices, State College, PA) interfaced with a personal computer (Hunter et al., 1998).

**Reliability statistic**

We developed a statistic \( R \) to compute reliability between \( N \) trains; \( N \geq 2 \). Let \( s_i \) be the \( i \)-th spike train, where bold face indicates a vector of spike times, i.e., \( s_i \equiv \{t_{i1}, t_{i2}, \ldots \} \). Let \( \mathbf{nn}_k \) be a vector of the nearest neighbors in train \( s_k \), \( k \neq i \), of each spike in \( s_i \); \( \mathbf{nn}_k \) and \( s_i \) are equal length. Defining the weight vector \( \mathbf{r}_{ik} = \exp(-|s_i - \mathbf{nn}_k|/\tau) \), where all operations are element-wise, gives a measure of the instantaneous reliability, for each spike in \( s_i \), with train \( s_k \). The quantities \( \mathbf{r}_{ik} \) can be used to measure dynamic changes in reliability, or can be averaged over to summarize the reliability of an entire response

\[
R = \frac{1}{N(N-1)} \sum_i \sum_{k \neq i} \langle \mathbf{r}_{ik} \rangle
\]  

(1)

where \( \langle \mathbf{r}_{ik} \rangle \) is the average value of the vector, a measure of the average reliability between \( s_i \) and \( s_k \). We chose a value of \( \tau = 2 \) ms for our measurements, which is comparable to the width of an action potential of the *Aplysia* motoneurons used in this study.
For the experimental data, slow drifts in firing rate between successive presentations of the stimuli sometimes occur; typically the spread of firing rates between presentations was 2-4% of the median firing rate. In order to reduce the impact of slow firing rate variations on the determination of spike time reliability, it is possible to compute $R$ by comparing only neighboring spike trains, i.e.,

$$R = \frac{1}{N-1} \sum_{i}^{N-1} \langle r_{ij+1} \rangle$$

As noted in the Results, this definition of $R$ results in a small improvement in the ability of the rate hypothesis to explain the synaptic control experiments.

A variety of methods have been introduced to quantify reliability and precision (Mainen and Sejnowski, 1995; de Ruyter van Steveninck et al., 1997; Hunter et al., 1998; Tiesinga et al., 2002). The method we use here has four primary advantages: 1) it is computationally efficient and conceptually simple, 2) the individual spike train responses can have time varying firing rates over any scale, 3) it is applicable to an arbitrary number of responses, including the case of only two responses, and 4) the statistic can be computed on a spike-by-spike basis allowing for the investigation of the temporal evolution of reliability.

**Phase locking protocols**

The motoneuron was stimulated with a sinusoidal plus DC input. The DC input was adjusted so that the motoneuron regularly spiked at a frequency $f_0$, and the frequency of the sinusoidal component, $f_s$, was varied. For each choice of $f_0$, $f_s$ we searched for regular patterns in neural spiking consistent with $n:m$ phase locking, i.e., patterns in which $m$ motoneuron spikes occur for every $n$ cycles of sinusoidal current ($n,m$ are integers). We minimized the effects of jitter on spike timing due to intrinsic noise by coarse-graining the time to 2ms bins. A spike train was identified as having a $n:m$ phase locking pattern if the observed pattern repeated for at least 10 action potentials. For every sinusoidal stimulus point, we also stimulated the motoneuron with a DC stimulus alone and computed the median firing rate in response to DC to estimate $f_0$ in the phase locking interval. The relative frequency, $f_s/f_0$, was obtained by dividing the sinusoidal frequency by $f_0$. The coefficient of variation of the sinusoidal plus DC input is $a_s/\sqrt{2}$, where $a_s$ is the amplitude of the sine wave divided by the DC component.

If a neuron was accommodating during the course of the experiment, we sometimes detected different phase locking solutions in different parts of the response with different values for $f_s/f_0$. In these cases the multiple values were plotted. A total of 1292 spike trains were collected from four animals, one neuron per animal.

**Leaky integrate and fire model**
The phase locking behavior of the leaky integrate and fire model has been thoroughly analyzed (Rescigno et al., 1970; Knight, 1972; Shimokawa et al., 2000; Tiesinga, 2002). The entrainment properties of this model to sinusoidal and aperiodic inputs are similar to those of vertebrate and invertebrate neurons (Hunter et al., 1998; Beierholm et al., 2001). The model's voltage between action potentials is given by the solution to

$$RC\frac{dV}{dt}(t) = -V(t) + R\left(I(t) + \sigma \xi(t)\right)$$  \hspace{1cm} (3)$$

where $V(t)$ is the membrane potential, $R$ is the membrane resistance, $C$ is the membrane capacitance, $I(t)$ is the coherent input current and $\xi(t)$ is Gaussian distributed white noise with zero mean and unit standard deviation scaled by $\sigma$. When the membrane potential reaches threshold $\theta$, the potential is instantaneously reset to rest. The model parameters for the leaky membrane and threshold were $R=5\Omega$, $C=10\text{nF}$, $\theta=45\text{mV}$, $\sigma=0.025\text{nA}$. The equations were numerically integrated using a 4-th order Runge-Kutta algorithm with an integration time step of 0.1ms.

In the special case that $I(t)$ is given by a spike train drawn from a periodically modulated Poisson process (see RESULTS), the input current was given by

$$I(t) = DC + i \times \left( \sum_k \delta(t - t_k) - \lambda_0 \right)$$  \hspace{1cm} (4)$$

where $\delta(t)$ is the Dirac-delta function, $t_k$ are the event times from the Poisson process with modulated rate $\lambda_0(1+msin(2\pi f_m t))$, $\lambda_0$ is the carrier rate, $f_m$ is the modulation frequency, $m$ is the modulation depth and $i$ is the event amplitude (Knox, 1970). Changes in the carrier rate affect the average firing rate of the neuron and hence the location of the resonance peak; the $\lambda_0$ offset removes this confounding factor. We used a value of $DC=10\text{nA}$ giving $f_0 \approx 8.7\text{Hz}$ with other parameters given in the figure legends. This frequency is within the physiological range at which many buccal neurons fire during feeding behavior (Church and Lloyd, 1994). From Campbell's theorem, a Poisson distributed point process $i\sum_k \delta(t-t_k)$ has mean $i\lambda_0$ and standard deviation $i\sqrt{i\lambda_0^2 + \lambda_0} / \Delta t$, where $\Delta t$ is the stepsize and the amplitude of $\delta(t-t_k)$ is 1/$\Delta t$. We used these equations to compute the coefficient of variation of the input currents.

RESULTS

Amplitude and frequency dependence of spike time reliability
Figure 1: Resonance effect for broad-band inputs is dependent on the relative amplitude. Two types of broad band inputs over three relative amplitude regimes are repeatedly presented to the *Aplysia* motoneuron. The first input, $+f_0$, is Gaussian distributed noise with a time constant of 4ms. The second, $-f_0$, is the signal $+f_0$ with the power around $f_0$ removed, and mean and standard deviation equal to that of $+f_0$. $R_+$ and $R_-$ below give the reliability for the signals with and without the frequency band $f_0$. A) CV=0.025; the noise-dominated regime - the reliability is dominated by the intrinsic noise and does not depend on the spectral content of the input $R_+=0.05$, $R_-\approx 0.06$, $f_0=12.3$Hz B) CV=0.15; the resonance-dominated regime - reliability depends on having $f_0$ in the power spectrum; $R_+=0.28$, $R_-\approx 0.10$, $f_0=16.3$Hz C) CV=0.35; amplitude-dominated regime - reliability is dominated by large amplitude fluctuations and both signals generate reliable spiking regardless of spectral content; $R_+=0.55$, $R_-\approx 0.53$, $f_0=15.1$Hz. In all cases we show ten superimposed voltage traces. Scale bars in panel C are 20ms by 20mV for voltage traces and apply to all traces. Currents are plotted as $(I(t)-DC)/DC$, where $I(t)$ is the fluctuating component, with the scale bar showing 20ms by 1 unit CV.

We use the term “resonance” when the spectral content of the input is an important determinant of spike time reliability. Figure 1 shows that the resonance effect for spike time reliability depends on the relative amplitude of the neural input. The relative amplitude of the fluctuations in the input current was calculated as the coefficient of variation (CV), i.e., the standard deviation of the fluctuations divided by the mean; our experiments examine the case where the mean is sufficiently large to trigger repetitive motoneuron spiking. The motoneuron is at rest at the onset of each stimulation, with a sufficient interval (30-120s) between stimulations to minimize effects from the previous stimulation.

In this experiment a single *Aplysia* motoneuron was repeatedly stimulated with the same aperiodic input. The term "frozen noise" has been used by Haas and White (2002) to describe aperiodic
signals used in the reliability protocol, i.e. protocols in which a single neuron is repeatedly stimulated with the same input. Two types of aperiodic signals were presented: 1) broad-band noise constructed by low-pass filtering Gaussian-distributed white noise and 2) the same signal with the frequency \( f_0 \) removed; see Hunter et al. (1998) for details. The signals were normalized so that the total power was the same.

For very small relative amplitude inputs (CV=0.025) neither signal generated reliable spiking (Figure 1A). When the relative amplitude of the aperiodic input was moderate (CV=0.15), the broad band signal containing \( f_0 \) generates higher reliability than the input lacking that frequency band (Figure 1B). In contrast, for a higher relative amplitude input (CV=0.35) the reliability is higher still and does not depend on the presence of \( f_0 \) (Hunter et al., 1998; Jensen, 1998, 2002). All three examples, A-C, are taken from the same motoneuron, and similar effects are observed across neurons and animals. Thus the importance of resonance phenomena in spike timing reliability is a function of the relative amplitude of the neural input.

**Modulated Poisson processes: three amplitude regimes**

![Figure 2](image)

**Figure 2:** *Modulated Poisson input current generates three relative amplitude regimes for spike time reliability.* A) Ten realizations of a periodically modulated Poisson process; \( m=0.4, f_m=8.7\text{Hz}, \lambda_0=10\text{Hz} \). B) Power spectrum \( S(f) \) from Equation 5. C) Spike time reliability of 40 leaky integrate and fire model neurons with a coherent “frozen” modulated Poisson process input \( I(t) \) and incoherent white noise input \( \sigma \xi(t) \); see Equation 3. Parameters: \( \lambda_0=200\text{Hz} \) equivalent to 20 Poisson inputs with a carrier rate of 10Hz, \( f_m=8.7\text{Hz} \) and \( 0 \leq m \leq 1 \). The average reliability for 20 simulations is plotted at each point. The CV’s from bottom to top are 0.01, 0.05, 0.1, 0.2, 0.4, 0.8, 1.6, 3.2. D) The same model and parameters but we hold the modulation depth constant at \( m=0.9 \) and vary the modulation frequency \( f_m/f_0 \) for three relative amplitude regimes: CV=0.01, 0.2, and 3.2. Only for the moderate amplitude input is a clear resonance peak seen around \( f_m/f_0=1 \).
A physiologically relevant class of signals to explore the relative amplitude dependence of spike timing reliability is the modulated Poisson processes (Tuckwell, 1989). These processes arise in the description of neural spike trains in which the probability of neural firing varies with time (Perkel and Bullock, 1968; Burkitt and Clark, 2000).

Here we consider spike train inputs drawn from a periodically modulated Poisson process. The advantage of this signal is that the power spectra and signal to noise ratio at the modulation frequency are known in closed form (Bartlett, 1963; Bayly, 1968; Knox, 1970). The modulation rate is given by

$$\lambda(t) = \lambda_0 \left(1 + m \sin(2\pi f_m t) \right)$$

where $\lambda_0$ is the carrier rate, $0 \leq m \leq 1$ is the modulation amplitude, and $f_m$ is the modulation frequency. It is assumed that the carrier rate is sufficiently low that the probability of spiking twice in a single time interval is small.

A realization of a neural spike train generated by a periodically modulated Poisson process is shown in Figure 2A and its power spectral density is shown in Figure 2B. The power spectral density, $S(f)$, is

$$S(f) = \lambda_0 + \lambda_0^2 \delta(f) + \frac{1}{4} \lambda_0^2 m^2 \delta \left( |f| - f_m \right)$$

where $\delta$ is the Dirac delta function (Knox, 1970). The broad-band, background power is the same at all frequencies and equals $\lambda_0$. The power at the modulation frequency is $\lambda_0^2 m^2 / 4$ and hence the signal to noise ratio is proportional to $\lambda_0 m^2$.

Figure 2C shows the spike time reliability for the leaky integrate and fire model stimulated by a periodically modulated Poisson process in the presence of noise. The ordinate shows the signal to noise ratio and the abscissa shows the reliability statistic $R$. Each point represents the average of 20 numerical trials for a given combination of $m$ and input CV. We applied a tonic current to offset the mean of the point process input, so that the neuron's average firing rate would be unaffected by carrier rate; see Equation 4. For all the points, then, the modulation frequency equaled the average neuronal firing rate; i.e., $f_0 : f_m$ was 1:1.

For each relative amplitude, there is a clear functional relationship between the reliability and the signal to noise ratio. For small relative amplitude inputs ($CV < 0.05$), the function is low and flat, 2) for large relative amplitude inputs ($CV > 1.6$), it is high and flat, 3) and for intermediate values there is a monotonic relationship between $\lambda_0 m^2$ and $R$. An analogous effect is seen if the modulation depth is held constant and the modulation frequency is varied: there is a resonance peak only for moderate amplitude inputs; Figure 2D. Thus a resonance effect is only observed when the relative amplitude of the input is moderate.
**Phase locking and reliability of Aplysia motoneuron with sinusoidal input**

![Diagram](image)

**Figure 3:** *Phase locking and reliability: Arnold tongue diagram.* A) Phase locking. A single sinusoid was presented to the neuron and the phase locked solutions for $n, m \leq 5$ are shown as a function of normalized frequency. The points with no phase locking are not shown. Of 1292 stimuli, we detected 645 phase locked solutions. The solid lines suggest a boundary for the Arnold tongue diagram for $n:m$ solutions with a sufficient number of points to suggest the outline of the tongue. The colors code $n$ and the symbols code $m$. black=1, red=2, blue=3, purple=4, green=5; *=1, • =2, ■ =3, ♦ =4, × =5; e.g., a red ■ is 2:3 phase locking. B) Reliability. Each of 526 stimuli were presented twice and the reliability of the response was measured using Equation 1. The tongues from A are superimposed for comparison. The same set of spike trains were used to compute A and B, with the repeated stimuli used to compute reliability in B used as separate spike trains to compute phase locking in A, though the number of stimuli is not the same in both plots because of different inclusion criteria. The colorbar ranges from $R=0$ to $R=1$.

The features of the amplitude-dependent resonance shown in Figure 2C can also be identified from measurements of reliability in a regularly spiking neuron receiving a periodic input (Figure 3). When the input to a regularly spiking neuron is itself periodic it is possible that the neuron can become entrained to the input. In particular for some modulation amplitudes and frequencies, for each $n$ cycles of the stimulus there are $m$ cycles of the spontaneous rhythm, i.e., $n:m$ phase locking (Glass *et al*., 1980; Guevara *et al*., 1981; Keener *et al*., 1981; Hayashi *et al*., 1983; Pakdaman, 2001; Szücs *et al*., 2001; Jensen, 2002) An Arnold tongue diagram is a summary of the phase
locking patterns as a function of the relative frequencies of the two oscillators and the coupling strength, here the amplitude of the input, between them.

Figure 3A shows the phase locking patterns from regularly spiking *Aplysia* motoneurons stimulated with sinusoidal input, and Figure 3B the reliability of the resulting spike trains. The amplitude of the sinusoidal input has been normalized to the magnitude of the DC current step, labeled as $a_s$ in Figure 3. For the sake of comparison the tongue boundaries obtained from Figure 3A have also been indicated in Figure 3B. While reliability is generally highest inside the 1:$m$ tongues, the results do not agree precisely: some points inside the tongues show low reliability (blue), and some points outside the tongues are high (red).

Re-examining Figure 3B in light of the results of Figure 2C, we can see that there are three qualitatively different behaviors in reliability that depend on the amplitude of the input. When $a_s < 0.05$, the effects of intrinsic noise dominate and there is no reliability for any input frequency. When $a_s > 0.35$, practically all frequencies are capable of generating reliable spike trains. In contrast, when $0.075 < a_s < 0.2$, reliability depends intimately on the relationship between the sinusoidal input frequency, $f_s$, and the intrinsic motoneuron spiking rate, $f_0$.

Phase locking and reliability are related but not equivalent. Phase locking is determined by examining the phase of the stimulus at which an action potential occurs, whereas reliability depends on the time that the action potential occurs. For $n:m$ phase locking, there are $n$ different time solutions, all of which have the same phase solution (Hunter *et al.*, 1998; Pakdaman, 2002; Tiesinga, 2002; Tiesinga *et al.*, 2002). For this reason, in the presence of intrinsic neural noise, it is expected that the 1:$m$ phase locking regions will generate the most reliable spike trains; compare the 1:2 solution with the 3:2 solution in Figure 4. The 1:1 phase locking region is the most robust in the presence of noise (Knight, 1972).

The results in Figure 4 show that phase locking outside the 1:$m$ tongues does not imply high reliability. The converse is true as well: high reliability does not imply phase locking. This is because spike time reliability depends on the intrinsic noise in the neuron. In the absence of noise, different trials with the same initial conditions will be perfectly reliable. However, they may not be phase locked, eg, if the input is quasiperiodic (Hayashi *et al.*, 1983; Tiesinga, 2002).
Figure 4: Phase locking and reliability for three periodic inputs in the leaky integrate and fire model. In all columns a sinusoidal input with $a_s=0.1$ was repeated 50 times in the model neuron with random initial conditions and no noise. The plots are taken from data in the last second of a 3s stimulus. The first three rows are 3 example spike trains from the 50, with the spike times superposed on the currents. The fourth row shows the raster plot of the spike times of all 50 responses. These plots only show the last second of a 3s stimulus, discarding the transient response. The bottom row shows the phase density histogram. A) $f_s/f_0=0.5$ generates 1:2 entrained firing and high reliability. B) $f_s/f_0=1.5$ generates 3:2 entrained firing but reliability is decreased because there are 3 time solutions C) $f_s/f_0=1.59$ does not entrain the neurons and reliability is decreased further.

Controlling reliability with synaptic and DC hyperpolarizing input

The above results demonstrate that for moderate relative amplitude aperiodic or periodic neural inputs, spike time reliability is determined by resonance between the intrinsic neural spiking rate and the spectral content of the input. Since spiking rates can be readily altered by synaptic inputs and neuromodulators, the ability of a neuron to support a spike timing code may be under active control (Hunter, 2001; Hunter and Milton, 2002). We investigated this possibility by measuring spike time reliability when the input to the motoneuron is the same, but the motoneuron spiking frequency is changed by either injecting a hyperpolarizing current or with inhibitory synaptic input from the B4/5 interneuron. A change in the firing rate of the motoneuron corresponds to a horizontal movement in the Arnold tongue diagram, and can be used to drive the system onto or
off of a tongue, i.e., from a region where reliability is high to one where it is low, and vice versa. We show that this mechanism can generate dramatic changes in reliability with only small changes in neuronal firing rates.

Figure 5A shows the repeated voltage responses of a motoneuron driven to tonic firing with a constant current and stimulated with a sine wave with parameters $f_s/f_0=1.05$ and $a_s=0.08$. This point lies on the high reliability 1:1 tongue. Figure 5B shows the same neuron with the same parameters, except $f_s/f_0=0.76$, located to the left of the 1:1 tongue. By applying a step hyperpolarization (Figure 5C), the relative frequency in both cases is increased, driving the neuron off the tongue in Figure 5A, and onto the tongue in Figure 5B. The resultant decrease (A) and increase (B) in reliability are evident, showing that reliability can be controlled over a time scale of tens of milliseconds with small changes in neuronal firing rate. This sensitivity to firing rate is seen only in the moderate amplitude regime. Note that although the spikes in the entrained regions of Figure 5A and B appear more reliable than those in Figure 1C, they are not: the appearance is due to the difference in time scales. For example, even though the spikes are aligned in the first half of the response in Figure 6A, there is still considerable jitter in the spike times at the time scale of 2 ms.

In Figure 6, we utilize the buccal interneuron B4/5 to alter the firing rate of a motoneuron receiving a sinusoidal input. B4/5 is a cholinergic interneuron presynaptic to most of the identified motoneurons in the ganglia, with well characterized synaptic dynamics (Gardner, 1990; Kehoe and McIntosh, 1998; Hunter and Milton, 2001). We stimulated the motoneuron shown in Figure 5 with the same pair of sinusoidal inputs, using the interneuron shown in Figure 6C to control the relative frequency of the interneuron and the sinusoid. The frequency of interneuron firing was chosen to

![Figure 5: Changes in spike timing reliability following a DC hyperpolarizing input. An Aplysia motoneuron was stimulated to regularly spike with a DC=13nA current and superimposed sine wave. In A), the sine wave before hyperpolarizing current onset had frequency $f_s/f_0=1.05$ and amplitude $a_s=0.08$. At 3.5 s, a step hyperpolarization was applied decreasing $R$ from 0.35 to 0.08. In B) the sinusoidal frequency was $f_s/f_0=0.76$, and the hyperpolarization increased $R$ from 0.10 to 0.4. A and B show ten superimposed voltage traces. The voltage scale bars are both traces and are 200 ms by 20 mV.](image-url)
generate an average firing rate change equivalent that caused by the hyperpolarizing DC current injection used above. In addition, we stimulated the interneuron with a sinewave (not shown) equal to its firing rate to phase lock it and regularize it’s firing between trials and reduce its spike frequency accommodation. The changes in reliability caused by interneuronal stimulation parallel those seen in the hyperpolarizing direct current stimulation.

**Figure 6:** Changes in spike time reliability following inhibitory input from B4/5 interneuron. A-B) As in Figure 5. C) At 3.5s the interneuron was stimulated to fire with a DC input of 40nA and a sinusoidal current to at 1:1 with interneuron firing rate to regularize firing between repetitions. The frequency of interneuron firing was calibrated to effect a rate change equal to that caused by the hyperpolarizing current in Figure 5. Onset of interneuron firing in A) decreased reliability from 0.36 to 0.28 and in B) increased reliability from 0.10 to 0.48.

Figure 6 shows that synaptic input can cause changes in spike timing reliability consistent with the results from the Arnold tongue diagram. Activating the interneuron and slowing motoneuron firing can either increase or decrease reliability depending on the motoneuron relative firing rate $f_s/f_0$. However, synaptic input can have effects on spike time reliability in addition to the rate effects. Notably, the IPSPs can entrain motoneuron firing as well (Pinsker, 1977; Kopell and Ermentrout, 1988; Cobb et al., 1995; Coombes and Bressloff, 1999; Hunter and Milton, 2002.

In order to determine the relative importance of these two effects on spike time reliability, i.e., rate control and synaptic entrainment, we altered motoneuron firing with both a hyperpolarizing and a synaptic input for $N=20$ experiments in 3 animals, and measured the change in reliability induced by both stimuli. For each of these experiments, the frequency of interneuron firing was calibrated to induce a rate change comparable to that caused by the DC hyperpolarizing stimulus. One of these 20 experiments is shown in Figures 5 and 6. The pure rate control experiments (DC hyperpolarization) explained 52% of the variance in the synaptic control experiments. Part of the remaining variance is presumably due to slow drift in neuronal state between stimulus repetitions. If we reduced the effect of firing rate drift between stimulus presentations by computing the
reliability only for neighboring spike trains (Equation 2), the rate control experiment account for 61% of the variance in the synaptic control experiments. The remaining variance in the reliability changes due to synaptic stimulation is presumably due to entrainment to the IPSPs, which is evident in Figure 6B.

**DISCUSSION**

We have demonstrated that the resonance effect for spike timing reliability critically depends on the relative amplitude of the fluctuating component of the input calculated as the coefficient of variation. For very small relative amplitude inputs, reliable spike timing is not possible because the noise determines spike timing. When the fluctuating component of the input is very high, reliability is high. This reliability does not depend on $f_0$, but rather on the presence of large amplitude, high frequency fluctuations, which cause rapid membrane depolarizations (Mainen and Sejnowski, 1995; Nowak et al., 1997; Cecchi et al., 2000). This observation is consistent with the Arnold tongue diagram, in which nearly all frequencies of sufficient amplitude ($a_s$) can phase lock neural firing. For intermediate relative amplitudes, however, resonance effects dominate. The quantitative CV values that determine the relative amplitude regime vary from system to system, and depend on intrinsic neuronal properties and the magnitude of the incoherent noise. Note also that our results do not address the case where the tonic driving current is subthreshold or where the membrane has subthreshold oscillatory dynamics; in these cases it is likely that other mechanisms govern spike time reliability (Pei et al., 1996; Haas and White 2002). However, that these three relative amplitude regimes occur both in models of noisy integrate-and-fire neurons and in invertebrate neurons receiving periodic, aperiodic and synaptic inputs strongly argues for a broad applicability.

Although our rate control experiments concentrated on changes in spike timing reliability to periodic inputs, numerical simulations using modulated Poisson inputs clearly indicate that the observations can be generalized to aperiodic inputs. The power spectrum of this aperiodic synaptic input plays the same role in spike timing reliability as it does for aperiodic Gaussian-distributed colored noise (Hunter et al., 1998; Jensen, 1998; Haas and White, 2002). We anticipate that there will also be resonances to the case of aperiodic inputs constructed as so-called doubly stochastic Poisson processes, i.e, a Poisson process modulated by an aperiodic process (Bartlett, 1963).

Our studies do not address which relative amplitude regime is used to generate reliable spike timing in vivo. Since the relative amplitude and frequency content of neuronal inputs continually varies (Jagadeesh et al., 1992; Steriade et al., 1993; Wilson and Kawaguchi, 1996), it is quite likely that both amplitude-dominated and resonance-dominated mechanisms are possible. Intuitively, the amplitude-dominated mechanism would be expected to arise in situations in which large populations of neurons must spike with very high reliability and precision, such as in response to the temporal binding of sensory stimuli (Engel et al., 1997) or in response to the generalized rhythms of sleep and consciousness (Contreras et al., 1996). Several of the studies noting the importance of high frequency stimulus power (Mainen and Sejnowski, 1995; Schneidman et al., 1998; Cecchi et al., 2000) have worked primarily in what we term the high amplitude range. On the other hand the greater flexibility of the resonance-dominated mechanism for spike timing reliability is quite seductive. Depending of their intrinsic firing frequencies, neurons can respond with either spike time or rate codes, or both. Rate dependent regulation of
spike timing is an alternate mechanism to support encoding with transient synchronizations (Abbott, 2001; Hopfield and Brody, 2001).

Motoneuron spike timing is an important aspect of the invertebrate control of motor activity. For example, invertebrate muscle contraction is sensitive to changes in the temporal pattern of neural spike trains (Wiersma and Adams, 1950; Gillary and Kennedy, 1969; Cohen et al., 1978; Wachtel and Kandel, 1971; Brezina et al., 2000a; Brezina et al., 2000b). In the Aplysia buccal ganglion, identified motoneurons have a common inhibitory input from B4/5 (Gardner and Kandel, 1977), continue firing while B4/5 is active (Church and Lloyd, 1994), and can fire synchronously during feeding-like behavior (Hunter, 2001). Thus the B4/5 interneuron is ideally placed to control motoneuron spike timing: with just small changes in rate, the reliability of spike timing of the muscle's neural input can be changed dramatically.

Aplysia has a comparatively simple nervous system, yet the complexity of the motor behaviors that can be generated is impressive. Our studies suggest that the organism has at its disposal an equally rich array of possible motoneuron spiking patterns that differ with respect to spike timing reliability. With just small changes in rate or input amplitude, the precision of timing of a motoneuron's neural input can be changed along with its correlation to other motoneurons (Vaadia et al., 1995). Moreover, it is possible that the same neuron can be either a rate encoder or a spike time encoder, or both simultaneously. The consequences of these different correlations of motoneuron activity on behavior remain to be determined, but likely depend upon the biomechanical properties of the organism, such as the size, geometry and arrangement of the muscles, the mechanical properties of the tissues, and the effects of the organism's environment on its movements.

Mazurek and Shadlen (2002) have shown how correlations in neuronal inputs can limit the ability of neuronal populations to encode a time varying input with population rates. Our results suggest the converse is true as well: small changes in firing rate of an uncoupled population of neurons receiving a coherent input affect the population's ability to synchronize to that input. Thus rate coding and spike time coding are intricately intertwined. We anticipate that the fact that neural spike timing can be so readily and rapidly controlled may facilitate not only the development of novel paradigms to study the effects of different patterns of neural activity on motor control but, also the design of brain stimulators to treat patients with medically intractable diseases of the nervous system (Milton and Jung, 2002).
Acknowledgments
Lyle Fox and Phillip Lloyd provided invaluable assistance with the experiments. John Crate assisted in the design of the electronics for these experiments and the computer hardware interfacing. We thank Jack Cowan, Nancy Kopell and Paul Tiesinga for useful discussions. We thank the reviewers for their useful comments. Research was supported by grants from the National Institutes of Mental Health and the Brain Research Foundation.
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