Cortical Brain States and Corticospinal Synchronization

Influence TMS-evoked motor potentials

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Running Head: EEG and EMG State and Synchronization Influence MEP

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Abstract

Transcranial magnetic stimulation (TMS) influences cortical processes. Recent findings indicate however that, in turn, the efficacy of TMS depends on the state of ongoing cortical oscillations. Whereas power and phase of electromyographic (EMG) activity recorded from the hand muscles as well as neural synchrony between cortex and hand muscles are known to influence the effect of TMS, to date, no study showed an influence of the phase of cortical oscillations during wakefulness. We applied single-pulse TMS over the motor cortex and recorded motor-evoked potentials along with the electroencephalogram (EEG) and electromyogram (EMG). We correlated phase and power of ongoing EEG and EMG signals with the motor evoked potential (MEP) amplitude. We also investigated the functional connectivity between cortical and hand muscle activity (corticomuscular coherence) with the MEP amplitude. EEG and EMG power and phase in a frequency band around 18 Hz correlated with the MEP amplitude. High beta band (~34 Hz) corticomuscular coherence exhibited a positive linear relationship with the MEP amplitude, indicating that strong synchrony between cortex and hand muscles at the moment when TMS is applied entails large MEPs. Improving upon previous studies, we demonstrate a clear dependence of TMS-induced motor effects on the state of ongoing EEG phase and power fluctuations. We conclude that not only the sampling of incoming information but also the susceptibility of cortical communication flow depends cyclically on neural phase.

Keywords

EEG, EMG, Corticospinal Coherence, Power, Phase

Introduction

Cortical oscillatory activity plays a crucial role for information processing in the brain (Wang, 2010). Different frequency ranges of cortical oscillation are associated with different functions (Nunez and Srinivasan, 2010; Dalal et al., 2011) and with stimulus processing in different modalities (Thut et al., 2011).

Studies of visual perception indicate that near-threshold stimuli are more likely to be perceived when low-level visual cortex is in a desynchronized state, reflecting an
increased excitability of visual regions. For example, alpha band power (Hanslmayr et al., 2007) (Van Dijk et al., 2008; Romei et al., 2010) has been robustly reported to influence the perception of visual stimuli. These findings suggest that alpha rhythms (~10 Hz) reflect an excitatory–inhibitory balance, in which strong alpha band power indicates an inhibitory state (Klimesch, 2012) and predicts perception. Alpha band phase (Mathewson et al., 2009; Busch and Vanrullen, 2010) has been reported to influence the perception of visual stimuli as well. Thus, in addition to power, the phase of cortical oscillations critically influences perception. Similar effects have been found in auditory perception, which is influenced by theta and delta phase (~1–6 Hz; (Schroeder and Lakatos, 2009; Stefanics et al., 2010; Ng et al., 2012; Henry and Obleser, 2012), and in somatosensory perception, which is influenced by local beta band (10 – 40 Hz) power over primary and secondary somatosensory cortex (Lange et al., 2011). One current interpretation of these results is that ongoing oscillations create periodic windows of facilitated information processing (Busch and VanRullen, 2010; VanRullen et al., 2011). In a similar manner, cortical oscillations have been suggested to temporally organize incoming speech signals and thereby segregate information into smaller units (Giraud and Poeppel, 2012).

Ongoing oscillatory activity also influences the effect of TMS. TMS-evoked visual perceptions, so-called phosphenes, are perceived more readily when TMS is applied in a period of low alpha power compared to a period of high alpha power (Romei et al., 2008; Hartmann et al., 2011). Phosphenes are also more readily perceived depending on the phase of occipital alpha within 400 ms prior to TMS (Dugué et al., 2011). Siebner and colleagues (Siebner et al., 2004) showed that pre-conditioning the primary motor cortex with low frequency (1 Hz) transcranial direct current stimulation (tDCS) could modulate the MEP. Related to this, Bergmann and colleagues showed state-dependent modulations of MEP amplitude (Bergmann et al., 2012). During global depolarization, indexed by up-states of neocortical slow oscillations (<1Hz) as recorded by EEG, TMS evoked significantly larger MEPs compared to TMS during down-states. These studies showed that the state of the motor system influences the effect of TMS.

The motor cortex communicates with spinal cord neurons via synchronized oscillations in the beta band (Schoffelen et al., 2005). Cortical beta frequency power (18 Hz) influences the amplitude of the MEP (Schulz et al., 2013). Prior to TMS stimulation, posterior electrodes with an associated source in left parietal cortex exhibited a negative
correlation with MEP amplitude. In addition to cortical power, the phase of ongoing oscillatory EMG activity also influences the effect of TMS. Van Elswijk and colleagues (van Elswijk et al., 2010) showed that TMS-evoked synaptic input from the cortex to the hand muscles is most effective when it arrives at the rising flank of the EMG beta frequency (18 Hz) oscillation. The synchronization between EEG and EMG activity, quantified as the so-called corticomuscular coherence (Hari and Salenius, 1999), also influences the amplitude of a TMS-evoked MEP. Schulz and colleagues (Schulz et al., 2013) showed that reduced communication between cortex and hand muscles as marked by low corticomuscular coherence in the alpha band (5-15 Hz) is associated with small MEP amplitudes, whereas optimal communication was associated with large MEP amplitudes.

In summary, EEG power, EMG power and phase, and the synchronization between EEG and EMG signals have all been found to influence the amplitude of motor potentials evoked by TMS. However, to our knowledge no study reported a link between ongoing EEG phase and MEP amplitude during wakefulness. Given the ubiquitous role of oscillatory phase in windowing of stimulus processing, EEG phase should also influence the effectiveness of TMS in a quasi-periodic manner.

On the basis of the above-mentioned results, we speculated that the phase of cortical activity influences the effect of TMS stimulation on motor output. To test this hypothesis, we applied TMS pulses to the finger region of the left motor cortex and correlated cortical and muscle activity prior to a TMS pulse with the motor activity evoked by the pulse. In line with the results by Van Elswijk and colleagues (Schulz et al., 2013) and Schulz and colleagues (van Elswijk et al., 2010), we hypothesized that pre-pulse cortical beta band power and phase, measured with EEG over the primary motor cortex, influence MEP amplitude. We further hypothesized that pre-pulse EMG phase and power in the beta band influence MEP amplitude. Finally, we expected a linear trend in the influence of communication between cortex and hand muscle, as indexed by corticomuscular coherence in the alpha band, on MEP amplitude such that optimal communication entails larger muscular responses.
Materials and Methods

Participants: Twenty-five right-handed participants (mean age 24, range 18–31 years, 9 male) without a history of neurological or psychiatric disorders took part in the experiment conducted at the International Laboratory for Brain, Music, and Sound Research (BRAMS) at the University of Montréal. All participants gave their written informed consent and were compensated for their participation. The experiment was carried out in accordance with the ethical standards of the Declaration of Helsinki and was approved by the local ethical committee. All the accepted recommendations for the use and safety of TMS were applied.

The current data were collected as part of a larger research project (Timm et al., under review), investigating auditory self-generation effects of voluntary and involuntary movements and their relation to the sense of agency. In brief, the experiment consisted of a block-wise presentation of three voluntary conditions (“motor-auditory voluntary”, “motor voluntary” and “auditory voluntary”) and three involuntary conditions (“motor-auditory involuntary”, “motor involuntary and “auditory involuntary”). All conditions involved EEG recording and the “involuntary” conditions involved TMS. The “auditory involuntary” condition involved sham TMS with the TMS coil tilted by 90°. In the voluntary conditions, participants were instructed to press a button. In the involuntary conditions, we applied a single TMS pulse to the left primary motor cortex that elicited an involuntary finger movement of the participants, leading to a button press. The TMS-induced movements were similar but of course not identical to the voluntary movements. In all conditions the experimenter was present in the laboratory. Each of the six conditions was presented in four blocks of 45 trials (180 trials per condition). With 1080 trials (6 conditions × 180 trials) at an average duration of 3.5 s, the experiment took approximately 1 hour, excluding subject preparation and breaks. Blocks for voluntary and involuntary conditions were always followed by the respective auditory-only and motor-only blocks. Apart from this constraint, the order of the voluntary and involuntary conditions was counterbalanced across participants. We focussed on the “motor involuntary” condition in the current analysis. Whereas previous studies (van Elswijk et al., 2010; Schulz et al., 2013) required hand muscle contraction during which the stimulation occurred, participants in this study were asked to press the button at will in the “voluntary” conditions, but to rest the hand on the response pad.
in the “involuntary” conditions. Therefore, no instruction to contract the muscles was feasible.

EEG recording and TMS application: During EEG recordings, participants were seated comfortably and were instructed to move as little as possible and to fixate their gaze on a grey cross, displayed on a black computer screen, in order to reduce eye movements. Stimulus generation and acquisition of behavioural responses were controlled using MATLAB (The MathWorks, www.mathworks.com) and the Cogent2000 toolbox (www.vislab.ucl.ac.uk/cogent_2000.php). Participants were instructed to rest the index and middle finger of their right hand relaxed on a piezoresistive response pad controlled by an Arduino microcontroller board (www.arduino.cc). TMS pulses were applied every 2.5 to 4.5 s (mean 3.5 s). Only trials in which a response (i.e. change in force applied to the response pad) could be elicited were used for data analysis.

TMS was applied with a Rapid2 system with a hand-held 70-mm figure-eight coil delivering biphasic pulses (Magstim, www.magstim.com). A Brainsight 2 neuro-navigation system (Rogue Research, www.rogue-research.com) was used to aid localizing and verifying the TMS target position. We registered a magnetic resonance image of a template head to the head of each participant. The neuro-navigation system tracked the relative positions of the TMS coil and the participant’s head during the experiment and displayed anatomical locations on the template brain corresponding to the current coil position. The approximate location of the left primary motor cortex was identified on the template brain. Initially, the coil was placed at a 45° angle relative to the parasagittal plane (Mills et al., 1992). The biphasic pulse induces a M-shaped current waveform in the cortex. In the first phase, the biphasic pulse therefore induces an anterior-posterior current flow, which is reversed to posterior-anterior in the second phase, and again reversed in the third and fourth phase (Sommer et al., 2006). The position of the coil was then adjusted so that a TMS pulse produced a motor potential in the right first dorsal interosseous muscle. This muscle abducts the index finger and is involved in stabilizing the metacarpophalangeal joint and in the voluntary finger movement that participants executed when pressing the button. Muscle activity was recorded with an electromyography system integrated with the EEG system. The intensity of the TMS stimulation during the experiment was set to 110% of the smallest intensity that produced a motor potential and a visible finger movement. The threshold intensity was determined using an adaptive staircase paradigm (Awiszus, 2003).
Average motor threshold intensity across all participants was 83.36% of maximum stimulator output. Due to the increased distance between the TMS coil and the scalp introduced by the EEG electrodes, we used relatively high stimulator intensity. A trigger was generated whenever the exerted force (as measured continuously by the response pad) deviated by a set amount from the reference value, which was defined as the weight of the relaxed finger on the pad. Significant movements that led to button presses were elicited in 81% (standard deviation: 14.27%) of involuntary trials. Participants were instructed to hold their hand relaxed while TMS stimulation to avoid possible corrections of button presses, which were too soft. It is important to note that this instruction could be seen as a “no-go” task. Therefore, participants likely exerted a mild tonic force to keep the hand still.

Electroencephalographic activity was recorded continuously throughout the experiment with a SynAmps2 amplifier (Neuroscan, www.neuroscan.com) and TMS-compatible sintered Ag/AgCl electrodes from 64 positions on the scalp, including the left and right mastoid (M1, M2). Electromyographic data was recorded with the same amplifier system from right first dorsal interosseus muscle. In addition, a ground electrode was placed on the forehead, and a reference electrode was placed on the tip of the nose. Eye movements were monitored with bipolar recordings from electrodes placed above and below the left eye (vertical electro-oculogram, VEOG) and lateral to the outer canthi of both eyes (horizontal electro-oculogram, HEOG). The EEG and EOG signals were sampled at 2000 Hz with an online lowpass filter of 200 Hz. In clinical settings, an online lowpass filter of 2000 Hz is usually used. This was not possible in our recording environment.

Data processing: Epochs of 3 seconds around the TMS pulse were extracted from the raw data of the “motor involuntary” condition. A linear trend was removed from each epoch and power line noise was removed by rejecting the 60 Hz bin from the epoch’s spectrum using a discrete Fourier transform. Resulting epochs were inspected for artefacts and channels with excessive noise or flat lines were interpolated. The EMG signal was rectified and high-pass filtered (10 Hz, 4th order Butterworth filter, one pass). Subsequently, the peak of the TMS artefact was identified and trials with a temporal aberration were excluded. MEP amplitude was computed as the difference between minimum and maximum between 30 ms and 200 ms after the TMS artefact. The EEG and EMG signal was band-pass filtered for the frequency of interest (17 – 19 Hz, 8th-order
Butterworth filter, one pass). In order to extract power and phase angles, a Hilbert transform was computed on three cycles of the 18 Hz frequency of interest prior to the up-ramp of the TMS artefact. Power values were computed from the absolute of the Hilbert transformed signal. We could not determine the exact phase at which the pulse arrived, because the up-ramp of the TMS artefact required us to insert a small delay (5 ms) between the extracted phase and the recorded TMS pulse.

In order to evaluate the 18 Hz effect in relationship to other frequencies, we performed a broad-band analysis. Therefore, we computed power, phase and coherence on the Fourier transform of a single, three cycle wide time window between 2 Hz and 50 Hz in 2 Hz steps, tapered using a single Hanning window. This resulted in spectral smoothing of 2 Hz for each frequency. The computation of coherence is based on the cross-correlation of two signals and requires an estimate of variance. It can therefore not be performed on single trials (Bullock and McClune, 1989). Single trials were thus sorted by the MEP amplitude and partitioned into quartiles for the analysis of corticomuscular coherence. To investigate the influence of the intensity of communication between the first dorsal interosseous muscle and the brain on the resulting MEP peak-to-peak amplitude, we statistically analyzed the linear trend between corticomuscular coherence prior to TMS and MEP size. From the complex Fourier values, coherence was computed between all EEG channels and the EMG channel (see Fig. 1 for details). Preprocessing and time-frequency analysis was accomplished using the FieldTrip open-source Matlab toolbox (Oostenveld et al., 2011).

Statistical analysis: Single trial EEG and EMG data were correlated with the amplitude of the MEP of each single trial. Angular-linear correlations between phase and MEP amplitude were computed (Eq. 27.47, (Zar, 2010)) as implemented in the circular statistics toolbox for Matlab (www.mathworks.com/matlabcentral/fileexchange/10676). Because circular correlation values can only take values between 0 and 1, subject-wise correlation values were converted to rational arcsine units (RAU; Studebaker, 1985) prior to statistical analysis. Correlation between power and MEP amplitude were computed using the Matlab built-in function for Pearson’s linear correlation coefficient. Pearson’s correlation values were Fisher-z-transformed in order to assure a normal distribution. Correlation values between EEG data and MEP amplitude were tested against zero with an independent-samples t-test with Monte-Carlo randomization and cluster-based
correction for multiple comparisons (Maris and Oostenveld, 2007). Correlation values between EMG-data and MEP amplitude were tested against zero with a one-samples t-test. Coherence values were linearized and also converted to rational arcsine units (RAU) for the statistical analysis using linear tests. It was assumed that increased corticomuscular coherence in the pre-TMS period would lead to increased MEP amplitude. Therefore we statistically analyzed the linear trend between corticomuscular coherence prior to TMS and MEP size.

Results

We found a significant correlation between EEG beta frequency activity estimated for 3 cycles of oscillatory activity prior to the TMS pulse and MEP amplitude. Cortical beta frequency (18 Hz) phase prior to TMS onset in a fronto-central electrode cluster showed a significant correlation with MEP (rho ~ 0.2, p < 0.001, Fig. 2 A and C). As we had applied TMS to the left hand area, located approximately below the C1 electrode of the 10-20 EEG electrode system, it is of note that C1 was among the electrodes that showed the strongest correlations.

We also found a significant correlation between EEG beta band power and MEP amplitude. Beta frequency (18 Hz) power prior to TMS onset in a parietal electrode cluster showed a negative correlation with MEP (r ~ -0.1, p < 0.01, Fig. 2 B and D). We found a significant correlation between 18 Hz EMG phase and MEP (t(24) = 5.53, sd = 9.49, p < 0.001, Fig. 2 E). There was a no significant correlation between EMG power and MEP, (t(24) = 1.67, sd = 0.19, p = 0.11, figure 2 E). Therefore, we conclude that the power level was identical over trials and the current results are not due to a trivial effect of motor pre-activation.

A clearly bimodal distribution of MEP amplitudes was observed, when analyzing them with respect to beta oscillatory phase at time of TMS pulse: TMS on the peak or trough of the beta frequency oscillation (~90° and ~270°) led to the largest MEP amplitudes (Fig. 3). Stimulation at these “optimal” EEG phase angles was followed by a 34% increase in MEP amplitude compared to an angle of 0° (109.09 µV vs. 71.61 µV). Stimulation at the optimal EMG phase angle lead to a 17% increase in MEP amplitude (123.60 µV vs.
101.95 µV). A state of low parietal EEG beta frequency power was followed by a 14% increase in MEP amplitude compared to a state of high beta frequency power (105.44 µV vs. 90.40 µV).

The similarity of the EEG and EMG phase effect suggests that effective communication between cortex and hand muscles may increase MEP amplitude. To test this hypothesis, we divided trials according to MEP amplitude into four quartiles and computed corticomuscular coherence for three cycles of oscillatory activity in each quartile. Following our last hypothesis, we tested the hypothesis of a linear trend in which smaller values of corticomuscular coherence in the alpha band (10-15 Hz) would be associated with the smaller MEP. Contrary to our hypothesis, we did not find an effect in the alpha band, but post-hoc testing showed a linear trend in the high beta band (34 Hz, F(1,24) = 6.05, p < 0.05, uncorrected, Fig. 4). This incidental finding is not statistically significant after Bonferroni correction for multiple comparisons, but its centro–parietal topography fits with that of the linear relationship between alpha-band power and MEP described by Schulz and colleagues (Schulz et al., 2013). Thus, there was some indication that trials with optimal communication between cortex and muscle, as indicated by increased corticomuscular coherence, exhibited the largest MEP amplitude.

**Discussion**

The goal of the present study was to relate ongoing cortical oscillatory processes prior to neurostimulation with TMS to the amplitude of the motor evoked potential (MEP). Participants placed their right middle and index finger on a pressure-sensitive response pad while we recorded EEG and EMG data. During this relaxed period, we stimulated the contralateral primary motor cortex with TMS above the motor threshold to elicit a motor-evoked potential. We hypothesized, that 1) cortical beta band power, but also phase over the primary motor cortex influence MEP amplitude; 2) EMG phase and power in the beta band influence MEP amplitude; and 3) a linear trend of the effect of corticomuscular coherence on MEP amplitude in the way that optimal communication entails the largest muscular response.
Two important studies on the role of cortical states marked by slow oscillations indicate an influence of the neocortical state on TMS-evoked MEP amplitude (Siebner et al., 2004; Bergmann et al., 2012). To our knowledge no prior study established a relationship between local cortical oscillations and TMS-evoked MEP amplitude during wakefulness. We found a significant correlation between oscillatory phase in the beta band range, centered at 18 Hz, and MEP amplitude. The MEP amplitude varied depending on the phase of local beta band activity in a fronto-central electrode group. The stimulation was most effective at a phase of approximately ± π. A similar phase relationship, albeit only for the EMG signal, was reported by Van Elswijk and colleagues (van Elswijk et al., 2010). Previous results on the influence between the phase of cortical oscillations and visual (Mathewson et al., 2009; Busch et al., 2009) and auditory perception (Neuling et al., 2012; Ng et al., 2012; Henry and Oleser, 2012; VanRullen and McLElland, 2013) suggest a widespread relevance of the peak and trough phase in various, usually slower, oscillation frequencies for perception. The present results support the general notion that oscillatory phase acts as a periodic process that gates perception in primary sensory cortices (Busch and VanRullen, 2010) and higher order cognition (Giraud and Poeppel, 2012), but extend it to sensori–motor processes and, congruently (Engel and Fries, 2010), to the beta-band range: Our results demonstrate that beta band phase in the primary motor cortex gates incoming motor commands. Thus the same principle of periodic information processing may apply to the motor system.

EEG beta band power has been related to movement, with increased beta band power indicating an idling of motor cortex neurons (Pfurtscheller et al., 1996). In line with our hypotheses and previous results (Schulz et al., 2013), we found that decreased parietal EEG beta-band power correlated with increased MEP amplitude. The parietal topography of the correlation strength suggests a source in posterior parietal cortex, which might be related to attention and coordination (Culham and Kanwisher, 2001; Behrmann et al., 2004). An “active” cortical state as indicated by decreased parietal beta band power might represent a susceptible state open to information processing and stimulation (Jessen et al., 2012).

An alternative, but related, explanation for the effects in posterior parietal cortex could be the guidance and preparation of actions. A number of animal studies have shown direct connections between posterior and frontal cortical areas (Johnson et al.,
Moreover, Andersen et al. (Andersen and Buneo, 2002) have shown the presence of maps related to the formation of movement intentions. The parietal-frontal connections might serve as projections of intentions formed within posterior parietal cortex. An “active” cortical state as indicated by decreased parietal beta band power might thus represent a state in which an intention to move has already been formed.

EMG phase, but not power, in the beta band influences MEP amplitude

Aside from the influence of cortical oscillatory activity on MEP, we also found a strong correlation of the phase of muscular (EMG) oscillations in the beta-band phase with MEP amplitude, at the same frequency of 18 Hz. EMG power in the same frequency was not significantly correlated with MEP amplitude. A recent study (van Elswijk et al., 2010) also linked the phase of EMG beta-band activity to the MEP amplitude. As mentioned above, we found a similar relationship between the time point of stimulation and MEP amplitude. A phase of approximately ± π entailed the largest gain modulation. This finding underscores the role of beta band phase in cortical and muscular oscillations as a gating mechanism for information transfer.

Corticomuscular coherence and MEP amplitude

We analysed information transfer from cortex to hand muscle in the last step of our analysis. Functional connectivity is the basis of communication between distant cortical regions, but also between the cortex and distal muscles, and it can be expressed in corticomuscular coherence (Gross et al., 2004; Schoffelen et al., 2005). We found a linear relationship between corticomuscular coherence and MEP amplitude in the high beta band (30–35 Hz). The trials with the smallest coherence values also contained the smallest MEP amplitudes and trials with largest coherence values contained the largest MEP amplitudes. In contrast to our results, which show the strongest effect in the beta band, previous studies found correlations between MEP and corticomuscular coherence in the alpha band (Gross et al., 2002; Schulz et al., 2013). However, participants in these studies were engaged in an active task, whereas our participants were stimulated while keeping the hand relaxed. Muscle activity may shift the spectrum of corticomuscular coherence away from a rhythm related to mild tonic force in the beta band to an active suppression rhythm in the alpha band. This notion is consistent with the gating-by-inhibition framework (Jensen and Mazaheri, 2010). Whereas the individual correlations
between phase, power, and MEP amplitude are small they have consistent scalp 
topography and agree with the results of the coherence analysis. Participants were 
instructed to keep their hand relaxed in the blocks of trials we analysed, but to actively 
move the hand in the remaining blocks. It is therefore possible that subjects perceived 
this as a “no-go” task. In this light, the ongoing activity prior to TMS could reflect a tonic 
stabilizing force, which in turn influences corticomuscular coherence. Our results 
therefore may not generalize to experimental setups in which the target muscle is fully 
relaxed and does not generate measurable EMG activity. Corticomuscular coherence 
cannot be estimated without sufficient EMG activity. In the present data, the EEG and 
EMG power spectra are not flat and don’t exhibit the signature broadband or 1/f power 
spectra expected from noise. Thus, we conclude that the small yet present EMG activity 
has an influence on corticomuscular communication.

Taken together, our results indicate that neural and neuromuscular beta-band activity 
significantly influences the amplitude of the TMS induced motor response (MEP) on 
different levels. The local state of primary motor cortex at the moment of TMS 
stimulation, as expressed in beta-band phase and power, and the more global state of 
functional connectivity with hand muscles critically influence how the stimulus (here: a 
sweep of neural depolarization extraneously elicited by TMS) will be processed and 
transmitted. Our results show local power and phase effects in the low beta band, but 
corticomuscular coherence effects in the high beta-band. This poses stimulating 
questions on the functional roles of these frequency bands in sensorimotor processing.

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**Figure Captions**

Figure 1: Overview of the data analysis steps. We computed MEP amplitude from the difference between maximum and minimum amplitude following the TMS pulse. The raw EEG and EMG signals were bandpass filtered and Hilbert-transformed to extract instantaneous phase and power shortly before the onset of the TMS. Depicted on the left side are single trial data from the first subject. We used a Fourier transform to estimate the frequency and coherence spectra of EEG and EMG signals for three cycles per frequency. Depicted on the right side are group averages for power and phase at electrode C1 and coherence between electrode CP2 and the EMG electrode.
Figure 2: Results of the correlation analysis between EEG and EMG 18 Hz phase and power and MEP amplitude (circular–linear and linear correlations, respectively). Top row: Topographic distribution of mean correlation coefficients between 18 Hz EEG and EMG phase (A) and power (B) and MEP amplitude. Bottom row: Topographic distribution of statistically significant correlation clusters between 18 Hz EEG phase (C) and power (D) and MEP amplitude. Statistical comparisons were computed on RAU- or z-transformed data, respectively. T-values are masked for statistical significance. Circular-linear correlations are by definition only positive. Therefore, different color ranges are used for the circular-linear and linear correlations. Electrode C1, which is close to the TMS stimulation site and the hand motor area, is circled in (A) and (C). (E) Mean correlation coefficients (± SEM) for the correlation between EMG 18 Hz phase and power and MEP amplitude.

Figure 3: Single-trial MEP amplitude by EEG (electrode C1) and EMG phase. Electrode C1 was picked as exemplar, because it covers primary motor cortex and is located close to the site of TMS. The x-axis of the Phase-by-Amplitude plots depicts the phase of the 18 Hz oscillations. A phase of zero and ± π indicate the inflection points between peak and trough. Each single point represents a single trial. The same information is depicted on the polar plots, whereby each single trial is represented by a single line, the length of which represents the MEP amplitude. TMS stimulation at the peak or trough of the 18 Hz EEG (A) and EMG (B) oscillation elicited larger MEP amplitudes than at other time points during the oscillatory cycle.

Figure 4: (A) Linear relationship between the 34 Hz corticomuscular coherence in a centro-parietal sensor group and the MEP amplitude. (B) This trend was strongest in the high beta band between 30 and 35 Hz. (C) Increasing corticomuscular coherence in the beta band was associated with increased MEP amplitude. Electrode CP2 is circled in (A) and was used for illustrative purposes in (B) and (C).
A. Topography at 34 Hz

B. F-Values (± STD) at CP2

C. Coherence at CP2 (± SEM) by MEP Amplitude